

BACHELOR PAPER

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Dosimetry of Ir-192 brachytherapy sources

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Vienna, May 20, 2021

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Kurzfassung

In der radiologischen Therapie, im Besonderen in der Brachytherapie ist es erforderlich für jeden Patienten eine individuelle Bestrahlung durchzuführen. Für die erforderlichen Bestrahlungsberechnungen stehen Bestrahlungsplanungssysteme zur Verfügung. Diese unterliegen, aufgrund der hohen Anforderungen, speziellen Richtlinien und müssen regelmäßigen Überprüfung unterzogen werden.

Für diese Überprüfung stehen unterschiedliche Normen bereit. Diese Normen beinhalten derzeit für die Brachytherapie keine Vergleichsmessungen zwischen kalkulierten Planungswert und Bestrahlungswert, wie sie in der Teletherapie bereits verwendet werden. Um diese Vergleichsmessungen auch für die Brachytherapie umzusetzen, wird in dieser Studie überprüft, ob mit Detektoren, die bereits in der Teletherapie angewendet werden, Messungen auch im Brachybereich mit guten Ergebnissen möglich sind. Mittels dosimetrischer Messungen werden diese Daten erhoben, um die Plausibilität der berechneten Daten zu überprüfen.

Für die Versuchsreihe stehen High Dose Rate (HDR) Ir-192 Quellen zur Verfügung. Die Messungen werden mit zehn unterschiedlichen Detektoren sowie zwei Elektrometer von den Herstellern iba und PTW durchgeführt. Die Messungen erfolgen in Wasser-Phantomen. Es stehen drei unterschiedliche Phantome zur Verfügung, von denen zwei speziell für diese Versuchsreihe konstruiert und angefertigt wurden. Die erhobenen Daten werden mittels der berechneten Werte des Oncetra Brachy Planungssystems des Herstellers Nucletron/Elekta verglichen. Die Messergebnisse liefern sehr positive Ergebnisse.

Zusammengefasst lässt sich sagen, dass eine Anwendung der Detektoren auch für die Brachytherapie einsetzbar ist. Dies ermöglicht es, dass Vergleichsmessungen in der Abnahmenorm von Brachytherapie Einrichtungen mit aufgenommen werden können.

Schlagworte: Brachytherapie, Bestrahlungsplanungssystem, Ir-192, High Dose Rate (HDR), Detektoren

Abstract

In radiological therapy, especially in brachytherapy, it is necessary to carry out individual irradiation for each patient. Treatment Planning System (TPS) are available for the necessary radiation calculations. Due to the high requirements, these are subject to special guidelines and must be regularly checked.

Different standards are available for this review. These standards currently do not include comparative measurements between calculated dose and irradiation dose for brachytherapy, as they are already used in teletherapy. In order to implement these comparative measurements for brachytherapy as well, this study will examine whether measurements in the brachytherapy range are also possible with good results using detectors that are already used in teletherapy. By means of dosimetric measurements, these data will be collected in order to check the plausibility of the calculated data.

High Dose Rate (HDR) Ir-192 sources are available for the test series. The measurements are carried out with ten different detectors and two electrometers from the manufacturers iba and PTW. The measurements are carried out in water phantoms. Three different phantoms are available, two of them were specially designed and manufactured for this series of experiments. The collected data are compared with the calculated values of the Oncetra Brachy planning system from the manufacturer Nucletron/Elekta. The measurement results are very positive. In summary, it can be said that one application of the detectors can also be used for brachytherapy. This makes it possible to include comparative measurements in the acceptance standard of brachytherapy facilities.

Keywords: Brachytherapy, Treatment Planning System (TPS), Ir-192, High Dose Rate (HDR), Detectors

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Des Weiteren möchte ich die Personen hier erwähnen die mich während meiner Studienzzeit direkt wie indirekt unterstützt haben.

Meine Familie, die mir den Raum und die Zeit gab meinen Weg zu gehen, auch wenn die Begeisterung für mein Studium zu Beginn nicht so gegeben war. Ich weiß das ich in euren Augen dafür schon zu Alt war, ihr habt aber alle zu Beginn gewusst, dass ich meinen Sturkopf durchsetzen werde und die Sache auch durch ziehe.

Meine Freunde, die mich während den Höhen und Tiefen begleitet haben und mir immer mit Rat, Tat und Meinung zur Seite standen. Ich weiß bis zum heutigen Tage nicht wie ich mich bei jedem von euch jemals erkenntlich zeigen kann.

Meine Feuerwehrkolleginnen und Feuerwehrkollegen die auf ein paar helfende Hände die letzten Jahre verzichten mussten. Wenn alles vorbei ist stehe ich wieder an eurer Seite und unterstütze euch wieder nach Leibeskräften.

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1 Introduction

1.1 Problem area

In radiotherapy, to provide patients with optimal care, it is necessary to carry out extensive treatment planning. In the age of computers, medical physicists and technicians are supported by dedicated Treatment Planning System (TPS). Especially in brachytherapy, where the radiation source is positioned directly inside the body, by usage of applicators, the patient is exposed to a high radiation dose [1, p. 1], [2]. This requires precise treatment planning of the irradiation and thus places high demands on staff and equipment. To avoid errors, irradiation TPS are subjected to regular Quality Assurance (QA) tests, which are regulated by various standards. These QA tests are based only on recalculations or checks with existing data [3], [4]. Therefore it is planned to carry out QA measurements. For this purpose, different phantoms with simple geometry and different detectors will be used. By comparing the measured and calculated dose, errors in the TPS can be detected.

The problem described above gives rise to several hypotheses for the study:

- Is a regular change in quality control necessary at all?
- Are the calculations of the TPS at all comparable with measurements, as the detectors are used usually in teletherapy?
- How far do measured and planned doses differ?
- Based on the detectors available for measurements, which are the most suitable once?

In order to answer these questions, quantitative methods are used to collect data to check the plausibility of the calculated data. For this purpose, the measured data are compared with the calculated data to be able to determine the deviation. These differences is decisive. During these measurements, a guideline is to be developed on how the measurements are to be carried out. Independently of this bachelor thesis, the guideline will later be integrated into the QA. Thus, this bachelor thesis is the cornerstone for the amendment of the ÖNORM S 5296 [4].

1.2 Insight into the matter

1.2.1 Brachytherapy

The word brachytherapy (<gr.> [$\beta\rho\alpha\chi v$] brachy, <engl.> short) means short-distance therapy. This means that a radiation source is applied inside a localised tumour. The steep dose gradient of a radiation source is used. Near the source, the dose falls very quickly due to the inverse square law ($1/r^2$). This causes an increase in radiation in the vicinity of the tumour, but the surrounding tissue or organs are spared due to the steep fall-off [5, p. 123], [6, p. 580]. The purpose of this radiation enhancement is to damage the Deoxyribonucleic acid (DNA) in the human cell nucleus by means of ionising radiation. The aim of this targeted damage is to damage the tumour cells so irreversibly that it goes into cell death or suffers permanent cell cycle arrest. Cell cycle arrest is when cells are no longer able to divide due to their damage. The cell death itself does not appear immediately, the cell is still able to proliferate for a certain time, but mostly it has lost its ability to divide indefinitely, which is equivalent to apoptosis due to the DNA damage. For targeted damage of the tumour, doses of approx. 20 - 100 Gy are necessary; it is important that the dosage is adapted to the healthy tissue. Only the dose that does not cause serious radiation consequences in the healthy tissue but still is high enough to eliminate the tumour should be administered [7, pp. 25, 35]. [8, pp. 29–30]

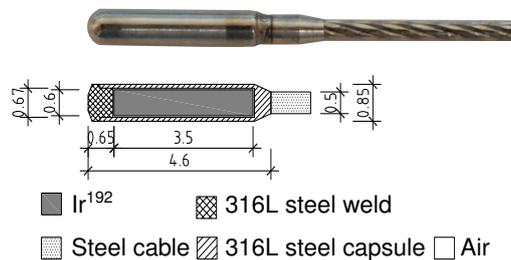


Figure 1: Structure of the Ir^{192} source with comparison to a photo of a dummy source. All dimensions are in mm (Source: modified taken from [9, p. 79]).

Various devices such as applicators, tubes and needles are available for guiding the source inside the patient. However, the core piece for successful brachytherapy is the afterloader. It contains the Ir^{192} source with the dimensions 3.5/0.6 mm (W/H) [9, p. 79]. This source is encased in a stainless steel capsule which is located at the end of a twisted steel cable. A picture with the dimensions of the source and a source cable can be seen in figure 1. The source itself is located in a safe in the afterloader. When irradiation is initiated, a dummy source first travels through the applicator. This is to check that the transfer tube and applicator are free of obstructions and of the correct length. Only then the source moves out of its safe and travels via the transfer tube to the applicator. The dummy source and the source are controlled by means of a stepper motors that can control step widths of 1 mm. It is also possible to move the source out via one of several channels. An picture of the Afterloader devices is shown in figure 2. [8, pp. 84–88]

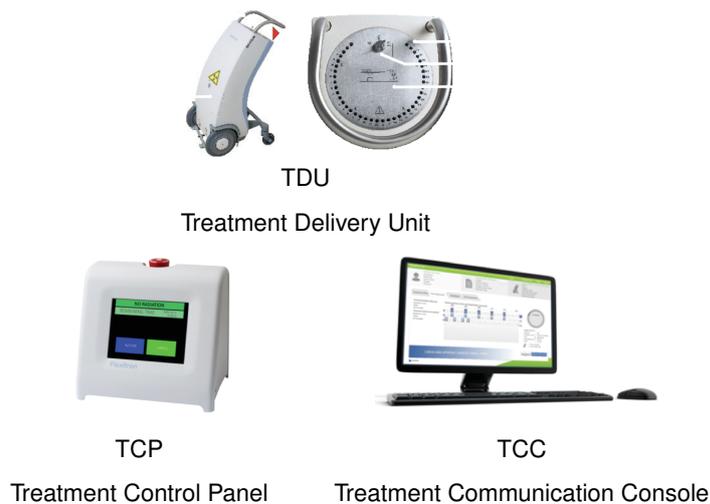


Figure 2: The Afterloader Treatment Delivery Unit (TDU) and his peripheral devices Treatment Control Panel (TCP) and Treatment Communication Console (TCC) (Source: modified taken from [10]).

1.2.2 Ir¹⁹² Source

In brachytherapy in particular, it is necessary to use different nuclides depending on the area of application. Whether irradiation is carried out by means of an afterloader or direct implementation in the body by means of seeds places different demands on the nuclide. For use in afterloaders, nuclides with a long half-life and high specific activity are preferred. Long half-lives allow the source to be in use for a long time, especially for nuclides that have to be produced artificially, a long usability represents a cost saving. A high activity makes it possible to produce very small-volume sources, which in turn make it possible to produce small and elastic source cables. Furthermore, it should be considered into which products the nuclide decays, as the decay products could also form radioactive substances. The most widely used isotope in brachytherapy in Europe is Ir¹⁹² [11]. Its half-life of 73.81 days and its high specific activity of 340.98 GBq mg⁻¹ qualify it for use in afterloaders [12, p. 5]. [8, pp. 34–35]

Ir¹⁹² is generated from an Ir¹⁹¹ nuclide and the (n,γ) reaction [13]. In the (n,γ) reaction, a thermal neutron is captured in a reactor by the target nucleus, in this case Ir¹⁹¹, forming a compound nucleus [14, p. 128]. By a thermal neutron Krieger et al. mentioned, that a "*neutron whose kinetic energy is of the order of the most probable thermal energy of a gas atom at room temperature*" [15, p. 203]. As a conclusion it can be said that a High Dose Rate (HDR) Ir¹⁹² source is created by Ir¹⁹¹ absorbing a neutron. [11]. Sources whose dose rate is higher than 12 Gy/h count as HDR sources [2].

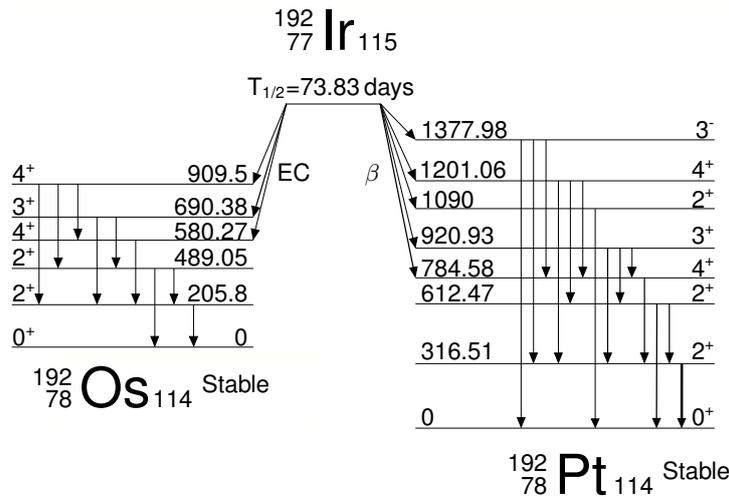


Figure 3: Decay schema of the radioisotope Ir^{192} (Source: modified taken from [16], [17]).

Ir^{192} decays by β radiation into platinum and by Electron Capture (EC) into osmium, both nuclides are stable [16]. During its decay, it emits 2.3 gamma rays per decay with an average energy of 0.355 MeV [13], [8, p. 35]. A decay schema with the exact energy levels can be seen in figure 3.

1.2.3 Treatment Planning System (TPS)

A TPS is defined in the standard Norm S 5295 as a programmable electronic system, which also includes all connected peripheral devices, that is used to simulate a radiation application to a patient. In practice, this means that calculations are made with calculation algorithms and stored databases that enable radiation planning. In addition to the special technical advances of recent years, Computed Tomography (CT) images of the patient can be fed into the TPS and thus optimise the treatment planning. Despite this progress, the formulas and data on which the calculations are based have remained largely the same. For TPS, the basis is Task Group No. 43 Report of American Association of Physicists in Medicine (AAPM). This report contains all the necessary formulae, including an explanation of them. Furthermore, for each radiation source of the different manufacturers a short description is given with a technical drawing as well as the tables with the data for the anisotropy function. The Klinik Donaustadt has an Oncentra Brachy TPS which calculates dose rate using the equation 1. [18], [9], [19]

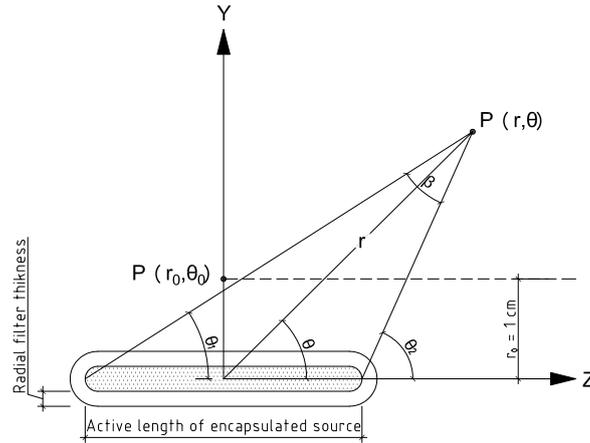


Figure 4: Geometry for the dose calculation formalism; see equation 1. $P(r, \theta)$ represent the Point-of-interest and $P(r_0, \theta_0)$ means the reference point (Source: modified taken from [11]).

$$\dot{D}(r, \theta) = S_k \Lambda \frac{G_x(r, \theta)}{G_x(r_0, \theta_0)} F(r, \theta) g_x(r) \quad (1)$$

$\dot{D}(r)$...Dose rate at point (r, θ) [$cGy h^{-1}$]

S_k ...Air kerma strength [$U = cGy h^{-1} cm^2$]

Λ ...Dose rate constant in a medium using air kerma strength normalization [$cGy h^{-1} U^{-1}$]

$G_x(r, \theta)$...Geometry factor at point (r, θ) [cm^{-2}]

$G_x(r_0, \theta_0)$...Geometry factor at point (r_0, θ_0) [cm^{-2}]

$F(r, \theta)$...Anisotropy function at point (r, θ) []

$g_x(r)$...Radial dose function []

The treatment planning for patients includes the determination of different volumes. The gross tumour volume is determined on the basis of image data and attention is also paid to the tumour spread area. This area most likely already contains tumour cells. Once the tumour region has been determined, the clinical target volume is defined, which includes not only the primary visible tumour but also all regions that could already contain tumour cells. In order to be able to intercept volume changes during treatment, a safety space is usually set up around the clinical target volume, this is called the planning target volume. Since tumours usually do not grow uniformly, the treatment planning must be adapted to this. This means that the planning target volume differs from the treated volume. The treatment planning also takes into account the irradiated volume, which includes all areas of the body that are unavoidably exposed to radiation due to the treatment even though they are not part of the planning target volume. [7, pp. 252–254], [6, pp. 489–490]

1.2.4 Detectors

Detectors are designed to produce a signal by physical or chemical reactions when ionising radiation is exposed. These can be divided into different groups based on the radiation effect produced [5, pp. 143–144]. Ionisation chambers use the effect of ionisation in gases for detection. Semiconductors and conductivity detectors have as main effect the ionisation in solids. Semiconductor detectors include the RAZOR^{Diode Detector} and the Semiconductor detectors from the manufacture PTW. The microDiamond is a conductivity detector, all other detectors used are ionisation chambers.

The main components of an ionisation chamber are the filling gas and the electrodes. The filling gas is usually air, as it is very similar to human tissue and water. When the filling gas is irradiated with ionising radiation, electron-ion pairs are created through interactions. In order to collect the primary charges generated by the ionisation of the gas and to detect them in the measuring device, it is necessary to apply a voltage to the chamber. An image of an ionisation chamber with the main components is shown in figure 5. [20, pp. 25–30], [5, pp. 145–148]

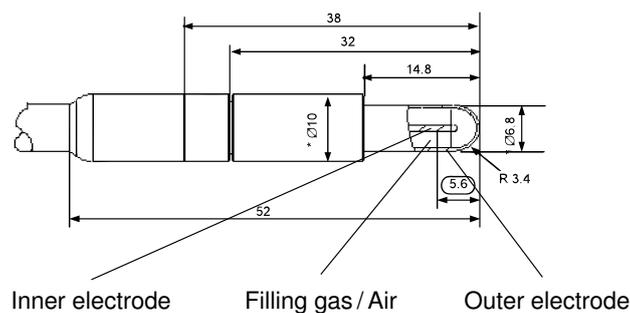


Figure 5: Cross-section view of an CC25 ionisation chamber. All dimension are in mm (Source: modified taken from [21]).

As already mentioned, the microDiamond is a conductivity detector, it consists of a synthetic single crystal diamond. Diamonds have the advantage that they are largely equivalent to soft tissue due to their low atomic number. When irradiated with ionising radiation, free electrons are produced in the conduction band, making the solid (diamond) conductive. This ionisation current can be detected by means of a measuring device. A special feature of conductivity detectors is the delayed signal detection when first irradiated. This is due to the traps (metastable intermediate level energetically between valence and conduction band) which must first be filled with electrons by means of pre-irradiation. Only when these free spaces are filled the ionisation can current flow undisturbed. [20, pp. 89–91], [5, pp. 173–175, 167]

Semiconductor detectors mostly consist of a p-i-n combination. These are diodes with a charge-free intrinsic zone. If a voltage is applied to the diode from the outside, the space-charge-free radiation-sensitive zone is formed inside. This zone acts like the volume of an ionisation chamber. [20, pp. 87–88], [5, pp. 170–172]

1.2.5 ÖNORM S 5296

The standard deals with the acceptance of TPS, whereby the acceptance takes place before the clinical commissioning. It is essential that an acceptance test must always be carried out when new radiation TPS are set up, or when essential components are changed. During the inspection, it is checked whether the TPS has been installed according to the manufacturer's instructions and is functional. Furthermore, it is checked whether the users are able to use the software without errors. In order to avoid subsequent errors, reference values are defined for the recurring weekly or monthly checks in the course of the acceptance test, to which the constancy tests must refer. [4]

2 Materials and Methods

2.1 Used Equipment and Detectors

The Klinik Donaustadt has two identical operating rooms, which two afterloaders. It is necessary to replace the sources in regular intervals. In the course of this change, the calibration data of the TPS were adapted to the new source. The calibration data of the sources used are listed in table 1 and assigned to the individual devices. The reference air kerma rate was measured by the department for quality assurance reasons. The results of the measurements chosen differences to the value of the certificate of -0.22 %, +0.38 % and +0.63 %, respectively.

Table 1: Calibration details of the three used Ir¹⁹² sources, specified by the production company Curium Netherlands B.V. The source in the Afterloader 1 device was change on the 22th of January.

Device	Calibration Date	Calibration Time	Reference air kerma rate $\left[\frac{cGycm^2}{h}\right]$	Apparent source activity $[Ci]$	Serial number
Afterloader 1	28.10.2020	18:04	52020	12.88676	NLF01D85E5606
	07.01.2021	03:12	44810	11.10065	NLF01D85E5930
Afterloader 2	02.03.2021	15:21	50810	12.58701	NLF01D85E6191

The used phantoms were commercially available phantoms and self-made ones. The self-made phantom called needle phantom and the in-vivo phantom are jigs made of Polymethylmethacrylat (PMMA) that are immersed into a small water tank. The needle phantom is 140/180/120 mm and the in-vivo phantom is 118/120/60 mm. The water tank is 695/503/595 mm (W/H/D).

The basic structure of a measurement setup consists of the afterloader, an electrometer, a phantom, a detector and the accessories required for the individual components. Each phantom can be combined with any electrometer and measurement detector, regardless of the manufacturer. In addition, all detectors are suitable for measurements in air and water. The detectors, with the exception of the RAZOR^{Diode Detector}, had a calibration certificate from the companies and thus also a calibration factor for Co⁶⁰. The Semiconductor probes had a calibration factor measured by the department itself with Ir¹⁹². The equipment for the various measurement setups is listed in table 2.

Table 2: List of the equipment and software used for the various measurement setups.

Device	Manufacturer	Model	Firmware version
Treatment Planning System (TPS)	Nucletron/ Elekta	Oncentra Brachy	4.6.0
Afterloader	Nucletron/ Elekta	Flexitron HDR Treatment Delivery Unit (TDU)	-
		Flexitron HDR Treatment Control Panel (TCP)	3.3.0.0103
		Flexitron HDR Treatment Communication Console (TCC)	3.3.0.0353
		Transfer tubes	-
		Application needles	-
Electrometer	iba	Dose ²	2.0.0.1
	PTW	Unidos T10001	2.40
Needle phantom	self-made	Needle phantom	-
In-vivo phantom	PTW	Multidose AL Box T16008	-
		Vividis T10018	2.40
		Multisoft	1.3
	self-made	In-vivo phantom	-
Water phantom	iba	Blue Phantom ²	-
		Water reservoir SMARTSCAN	-
	PTW	MP3 T4316	-
		MP3 Control Unit T41013	1.10
		MP3 Tandem T10011	1.10
		Water reservoir MP3 T43163	-
Mephysto-Software	3.4		
Detectors	iba	CC04	-
		CC13	-
		CC25	-
		RAZOR ^{Chamber}	-
		RAZOR ^{Nano Chamber}	-
		RAZOR ^{Diode Detector}	-
	PTW	0.3 cm ³ Semiflex Chamber T31013	-
		microDiamond T60019	-
		Semiconductor detector T9112 (Rectum)	-
Semiconductor detector T9113 (Bladder)		-	

2.2 Test sequence

2.2.1 In-vivo phantom setup

For measurements with the semiconductor detectors, it was checked whether the serial numbers of the boxes matched those on the detectors. Then the two semiconductor detectors were inserted into the in-vivo phantom. One probe was placed above and one below the application needle. The application needle was placed in the intended location in the centre of the phantom. The phantom was then placed in the plastic box. The internal dimensions of the box are 372/230/267 mm (W/H/D). The box was filled with water at room temperature until there was about 50 mm of water above the phantom. The needle was connected to the afterloader at channel five using a transfer tube. The two detectors were connected to the Multidos AL box. The finished measurement setup is shown in figure 6.

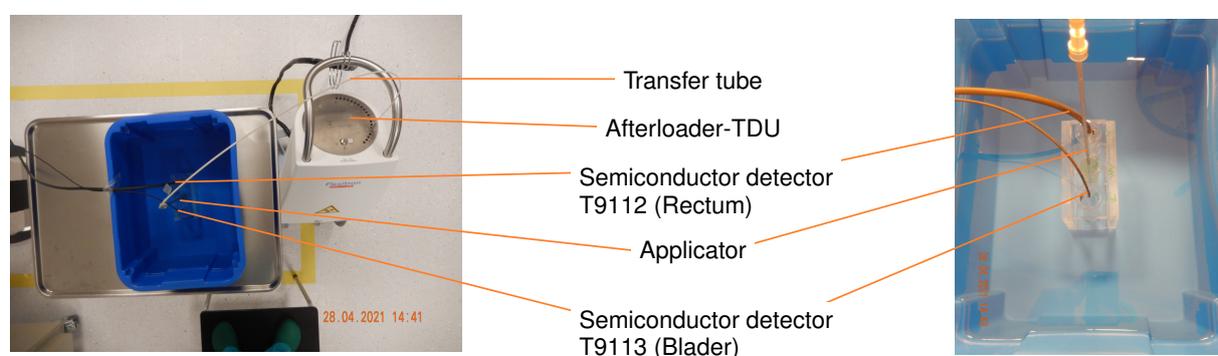


Figure 6: Measurement set-up with the in-vivo phantom.

The department has three sets of rectum and bladder probes (set A, B and C). The measurements were performed with probe set B. Since all the probe sets were created in the Multisoft programme, only the set that was connected to the Multisoft programme had to be selected. In addition, the range was set to "High". A previously prepared irradiation plan was now started at TCC. When starting the irradiation, the measurement of the radiation dose was started simultaneously in Multisoft. After the irradiation plan was executed and the TCC indicated that the irradiation was finished, the measurement in the Multisoft software was stopped and the measured values of the probes were saved as a Portable Document Format (PDF).

2.2.2 Needle phantom setup

First a thermometer and barometer was positioned in the operating room to measure the air pressure and room temperature. These values were required for the calculation of the correction factor of the air density and temperature (ρ_{TP}). Depending on the electrometer used, the chamber had to be created first with the calibration certificate, if available. The instructions in the manufacturer's operating manual were followed. The exact setting options and operation of the electrometers are described in the chapters "2.2.5 Timed continuous method" and "2.2.4

Timed collection method".

The needle phantom was placed in the centre of a plastic box. All four application needles were positioned. To check whether the needles were positioned correctly, the distance between the upper edge of the phantom and the end of the needles was measured. If this was 2.9 cm, the needles were correctly positioned. The box was then filled with water at room temperature until the upper edge of the phantom was reached. The transfer tubes were now connected to the needles and these were connected to the afterloader device (channel 1 to 4). Attention was paid to the sequence (needle one to slot one etc.).



Figure 7: Measurement set-up with the 4 needle phantom.

To prepare the detector, the serial number on the detector was compared to the one of the box. Since there are several identical detectors, the risk of mismatch was minimized. The serial number was used checking the calibration certificates and the measurement documentation. The detector was connected to the already warmed-up electrometer via an extension cable and the zero adjustment was done. During the zero adjustment, the protective cap was on the measurement chamber. The detector was then inserted into the fixing device without the protective cap until the indicator mark of the detector matched with the end of the fixing device. The different detectors had different indicator marks, an example is shown in figure 8. A screw was used to fix the detector in the fixing device. The device was then inserted into the phantom. The measurement setup is shown in figure 7.



Figure 8: Indicator marks of the chambers when positioned in the fixing device.

For the "90° 2 needle" measurements, there were two holes for the needles on the side walls of the phantom, you can see this setup in figure 9. The phantom was placed on a flat, hard surface

so that one of the side walls faced downwards with the holes. The two needles were then inserted into the holes one after the other until they were in line with the surface. The phantom was placed in the water basin in this orientation. Now the transfer tubes were connected one after the other. In order to position the detector correctly in the fixing device, the data of the existing maximum signal measurement and the position of the two needles were used. With a simple calculation, the position of the chamber could be determined and fixed in the fixing device through the screw. The detector was then inserted into the phantom. Then the chamber was connected to the electrometer and a zero adjustment was carried out. For each of the chambers, the positioning of the detector was recalculated and implemented.

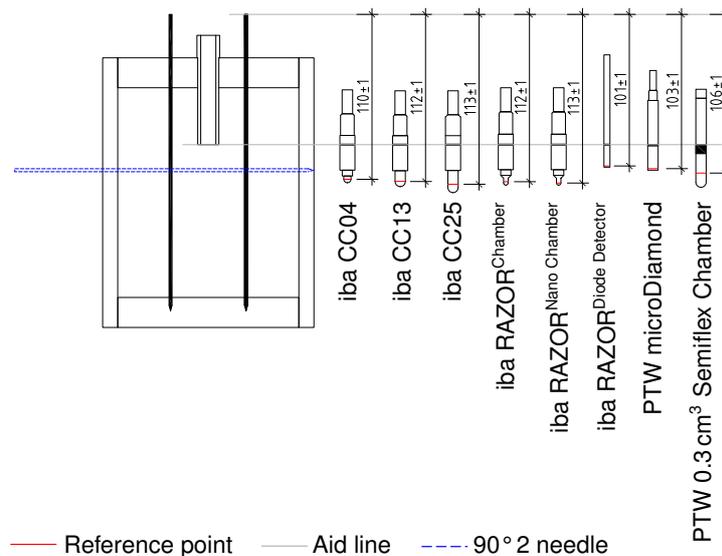


Figure 9: The needle phantom with the comparison of the ion chambers used. The detectors were always clamped in the fixture using a predefined indicator mark. Since the reference point (i.e. the geometrical center of the active volume or the effective measurement point) of the ion chambers is specified by the manufacturer, it can be determined at which extension length of the source the detectors have the highest sensitivity. Unit for the measurements is mm (Sources: influenced by [21]–[28]).

2.2.3 Water phantom setup

The basic measurement setup was the same for the two water phantoms, the Blue Phantom² from the company iba and MP3 from the manufacturer PTW. Since all but one of the measurements were done with the MP3 phantom, attention will be focused on this phantom.

The positioning of the needles was fixed to the water phantom in a designated and reproducible position. Figure 10 shows the setup. The needles were then inserted into the phantom. To check whether the needles were positioned correctly, the distance between the upper edge of the phantom and the end of the needles was measured. If this was 2.8 cm, each needle was placed correctly. The transfer tube was connected to the needle and to the afterloader. The

water was started to be filled from the water tank into the water phantom. To do this, the water tank was connected to the phantom and the pumping system was started. During the filling process the serial number of the ion chamber was checked against that on the box.

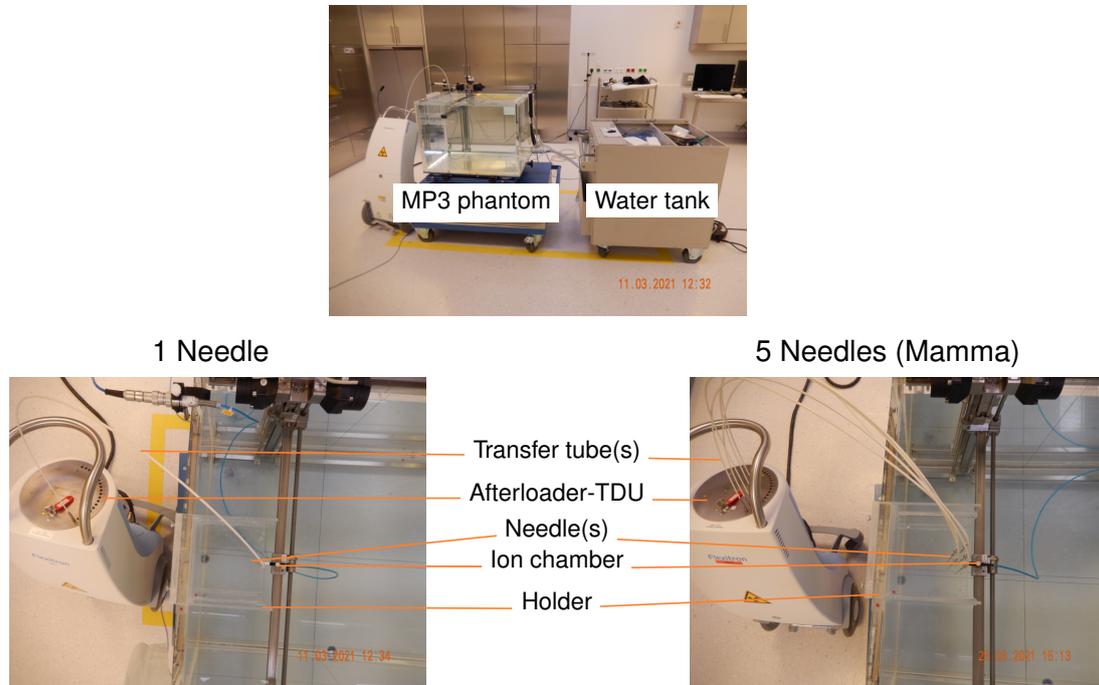


Figure 10: Measurement set-up with the Water phantom MP3 from the company PTW. In the top is the overview of the test set-up, the pictures below shows the construction in the water tank.

Next step was to insert the detector in the fixing device. The detector was inserted into the fixing device until the indicator mark of the detector matched with the end of the fixing device. An example of the different indicator marks is shown in figure 8. The microDiamond and RAZOR^{Diode Detector} in the fixation was screwed in horizontal position on the undercarriage of the water phantom, the ion chambers of iba was screwed on the undercarriage in vertically position, you can see this in figure 12. The detector was connected to the electrometer via an extension cable. The electrometer, and if necessary the detector, were warmed up. After the warm-up phase, the detector was added to the electrometer library. Than a zero adjustment was performed. In addition, the barometer and thermostat, which measured air pressure and temperature, was positioned in the operating room.

After the MP3 Phantom had been filled to the wanted water level, the pump system of the water tank was turned off. Now the MP3 Control Unit was connected to the control unit of the MP3 landing gear. In addition, the Control Unit and the MP3 Tandem were connected to each other. A control cable was positioned from the control unit out into the monitoring room and connected to the laptop on which the Mephysto software was installed. Since the radiation was measured with the electrometers and ion chambers, the Mephysto software and the control unit only served to control and to change the positions of the detectors inside of the phantom.

The position of the detector could be moved in three directions by means of the undercarriage. These correspond to the usual x, y and z axes, but are named A, B and C by the manufacturer PTW. It was important for the software to set a zero point. Using this zero point, it was possible to move in all three coordinates using positive and negative values. This is shown in figure 11, which also shows the different zero positions of the individual detectors.

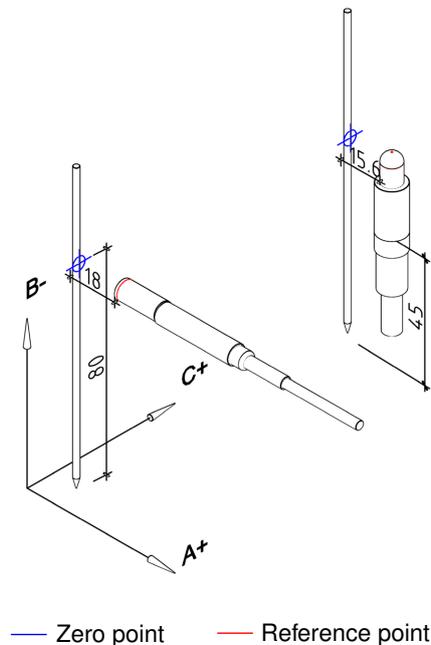


Figure 11: Coordinate axis for the Water Phantom. The absolute zero points is in the centre of the needle, the height varies depending on the ion chamber used. On the left in the picture you can see the PTW microDiamond, on the right the iba CC13 chamber at an A-coordinate of 20 mm. Due to the different reference points, the distance at A = 20 mm is also different. Movements of the detector in the A-axis enable depth dose measurements. B-axis motion make cross profile measurements possible. The C-axis was only use for 5 needles in triangular measurements. (Source: influenced by [23], [27]).

For a better understanding of the coming illustrations, it is important to explain two terms.

Absolute zero point: Centre of the radiation source and the reference point of the ion chamber when they overlap each other. A- and C-axis coordinates are both zero in this area, B-coordinate varies depending on the ion chamber. It is only a mathematical value.

Zero point: The range that can be set with the MP3 undercarriage. It is defined and stored in the control system as the zero point. All movements are carried out from there.

For defining and setting up the zero point of the microDiamond, the detector was moved to the needle until it touched the needle (A-plane). However, the needle should still be easy to move. This was to ensure that the pressure on the needle was not so high that the needle was bent. Then the detector was moved upwards from the needle tip to the centre of the needle until 80 mm was reached (B-plane). The height in the B-axis was measured using a rolling metre.

For alignment in the C-plane, it was visually checked whether the measurement chamber and needle were centred on each other (C-plane). The reference point of the ion chamber is 1 mm behind the probe head. Now, if an A-axis change of 20 mm was to be made, 18 mm was entered in the Mephysto system. This compensates for the 1 mm of the needle radius and the 1 mm of the detector to absolute zero. A picture of the zero point and the coordinates system for the microDiamond is shown in figure 11.

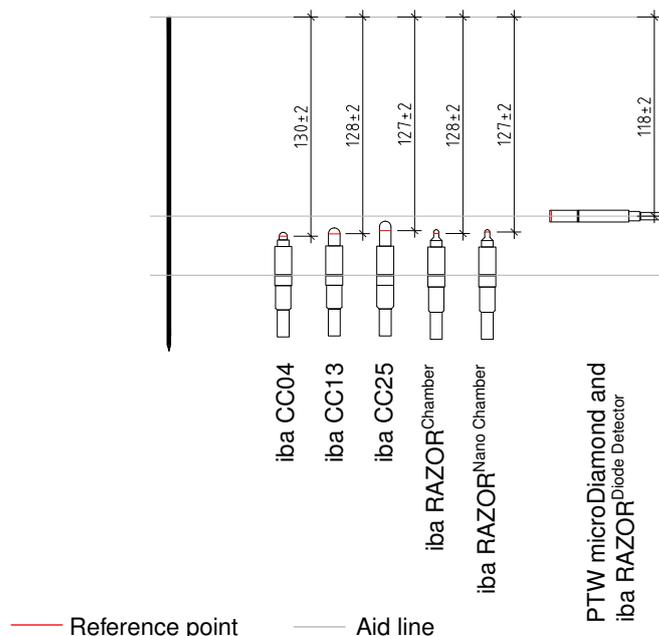


Figure 12: Representation of the detectors positioning in comparison to the needle location in the water phantom. The detectors were always clamped in the fixture using a predefined indicator mark. Since the reference point of the ion chambers is specified by the manufacturer, it can be determined at which extension length of the source the detectors have the highest sensitivity. Unit for the measurements is mm (Sources: influenced by [21]–[25], [27]).

The iba ion chambers were moved so close to the application needle that the centre of the needle and the centre of the detector were 30 mm apart (A-plane). This distance was checked using a sliding gauge. Then the ion chamber was moved in the B-axis until the indicator mark (black ring) of the detector was 45 mm away from the needle tip (B-plane). In the C-axis, the needle and detector were again only checked to see if they were aligned centrally (C-plane). This position was saved as the zero point. For the iba detectors, the reference point is located centrally in the probe head. However, since the adjusted zero point was 30 mm away from absolute zero, no mathematical corrections had to be made. The schema for the zero point for all iba ion chambers is shown in figure 11.

For position changes of the ion chamber, either the Mephysto computer control or the remote control of the phantom was used. The latter was only used to set the zero point. All coordinates in the results and tables always refer to the absolute zero point.

2.2.4 Timed collection method

This method was applicable to both electrometers of the manufacturers iba and PTW. If there were setting options that are only available on one of the devices, this will be explicitly indicated in the text.

After connecting the electrometer to the power supply and a warm up time, the ion chamber was created in the device library. This was done according to the operating instructions and all necessary data were taken from the calibration certificate of the detector, if available. The power supply for the chambers was set. For the iba detectors and the 0.3 cm³ Semiflex Chamber this was 300 V and for the microDiamond 0 V.

On the PTW Unidos, by selecting the detector in the library, the user is informed that the voltage will be changed to the value stored for the ion chamber. The voltage is only changed when the start button on the Unidos is pressed, any other button aborts the process.

Then the detector was connected. With the iba electrometer, we also had to choose which channel the detector was connected to, and we always used channel one. For the selection of the range "Low", was preferred, but for some measurements it was necessary to switch to "High", otherwise the electrometer would display an error message instead of the result, because the measurement results were outside the range. With iba Dose², X were displayed on the measurement display instead of values [29]. The PTW Unidos showed the error message "OL" on the display [30]. A measuring time was now set on the device, this was in the range of 6 to 200 s. The measuring times are always given in the result tables. At the afterloader TCC the irradiation time for each position was set to the measuring time plus 15 s.

After these preparations, the actual measurement was started. The irradiation was started, if the source was at the first position and already irradiated there for 1 to 2 s, the measurement was started on the electrometer. After the specified measurement time, the device displayed the measurement result. This was noted and the result was reset. The same procedure was followed for each further position that was irradiated.

The manufacturer's instructions for the various ion chambers had to be taken into account during preparation. Some detectors required pre-irradiation or a certain minimum dose. The pre-irradiation was always carried out before beginning of the measurement recordings by simply moving the source to a certain position and irradiating there for several minutes. In order to check whether the required dose had been reached (the microDiamond requires e.g. 5 Gy), measurements were taken. The irradiation dose was adjusted so that it never fell below the dose required that some of the detectors needed.

2.2.5 Timed continuous method

This method is again applicable to both electrometer models, if settings are only applicable to one model, this will be explicitly stated in the text.

At the beginning, the electrometer was connected to the power supply and the warm-up of the device was started. The ion chamber was then created in the library if it was not already present. If it was available, it was simply selected. Then the detector was connected to the electrometer.

By selecting the desired measurement detector in the library, one was asked on the Unidos whether one now wanted to change the voltage to the stored value, with the Start button this process had to be confirmed.

On the iba, the desired voltage was selected manually in the "Bias" menu and it could be read on the display whether this was also achieved. In addition, the slot to which the ion chamber was connected had to be selected for this device. Only channel one was used for the measurements.

Next, the range was set to "Low". The range was set to "High" only when needed. The measurement time was set to "continuous", which allowed an infinitely long measurement.

After preparing the measurement chamber and the electrometer, the programming of the irradiation plan was started or sent from the TPS to the TCC. First a test cable run was carried out by the afterloader, after completion of this test cable run, a click sound indicated that the test cable had arrived back in zero position. With this sound, the start button on the electrometer was pressed and the measurement started. Then the active source moved from the safe to the programmed position. After the irradiation schedule was completed and the source was returned to the safe. The electrometer was checked for a few seconds to see if the measurement result still changed. First, if the value remained stable, it was noted.

The same procedure was used for irradiation with several needles. Since a separate test cable run was always carried out for each needle, there was enough time to note the measurement result during this pause of irradiation. It should be noted here that the time on the electrometer continued to run permanently during the entire measurement. The measurement result was not reset at any time. The summed value was always taken. Only after all needles and positions had been irradiated and the TCC indicated that the irradiation was finished, the measurement was stopped on the electrometer.

2.2.6 Radiation and measurement procedure

Due to its technical construction and the extensive possibilities, the TDU is able to move the Ir^{192} source at any position inside the needle. Due to this fact, two possible radiation applications were used during the test series. On the one hand, the "point-source", where the source was moved to a predefined position and remained at this position during the entire measurement process. On the other hand, the "active length", where the source moved a defined distance inside the needle according to a treatment plan programmed in advance in the TCC. For both applications, it was necessary to define the positions in the needle and the dwell times in the positions. The needle itself has a length of 190 mm, in TCC it is possible to move the source the positions in millimetre steps.

"Point-source" irradiation was used in the needle phantom and water phantom for the measurements dose linearity of point-source, comparative measurements of 2 and 4 needles, point-source - Depth dose, Point-source - cross profile and dependance on water heights. "Active length" was applied in all three phantoms used and in the measurements not listed above. The exception was the comparative measurements of all detectors an one day, where both point-source and "active length" were used.

Another additional adjustment application is the water phantom. In contrast to the in-vivo and needle phantom, where the chambers are fixed rigidly in the phantom, the chassis of the phantom can be driven in three directions. The exact designation of the axes and the setting options have already been explained in detail in the chapter "2.2.3 Water phantom setup". For the measurements, driving with the chamber in three coordinates also resulted in three measurement possibilities. For the depth dose, the detector was moved away from the needle in the A-axis. The distance between the chamber and the needle could be increased millimetre by millimetre. In the cross profile, the detector was brought to a certain distance from the A-axis (= equilateral distance). Then the needle was moved along the B-axis by means of the chamber. Since millimetre positioning was also possible here, the entire length of the needle could be traversed. With the five needles in triangular configuration, the chamber was moved to an equilateral distance of 18 mm. Then the chamber was moved step by step in the C-direction so that the distance to the needle was increased further. The total of five setting options made the high number of different measurement methods possible.

3 Results

To calculate the correction factor for the air the equation 2 was used; this is specified in the standard Norm S 5234-2. There are two notations for the correction factor p_{TP} [31] and the k_P [32], throughout the document the notation of standard S 5234-2 has been used.

For all the presented tables "deviation" (equation 3) and "deviation of normalised data" (equation 5) were calculated. The "derivation" is the difference between measured dose and the calculated dose. For calculating the so called "deviation of normalised data" both, the measured and the calculated doses, were normalised to the dose in a specific point (equation 4) and then compared. This specific point dependent on the individual measurements, see table 3.

Table 3: Listing of the specific dose points for normalisation.

Treatment	Normalised to (Point X)	
	A-axis	B-axis
Needle phantom		
Dose linearity of point-source	Time per position 50 s	
Water phantom		
Dose linearity of point-source	Time per position 60 s	
Point-source - depth dose	20 mm	-
Point-source - cross profile	e.g. 10, 15, 20, 30 mm	0 mm
Active length - depth dose	20 mm	-
Active length - cross profile	e.g. 10, 20, 30 mm	0 mm
5 needles in triangular configuration	20 mm	-

$$p_{TP} = \frac{p_0}{p} \cdot \frac{T}{T_0} \quad (2)$$

p_{TP} ...Air density correction factor []

p_0 ...Reference air pressure 1013 hPa [hPa]

p ...Air pressure [hPa]

T ...Temperature [K]

T_0 ...Reference temperature 293.2 K [K]

$$Deviation [\%] = \left(\frac{Measured\ dose}{Calculated\ dose} \cdot 100 \right) - 100 \quad (3)$$

$$Normalised\ calculated/measured\ dose [\%] = \frac{Value \cdot 100}{Value\ at\ point\ X} \quad (4)$$

$$Deviation\ of\ normalised\ data [\%] = Normalised\ calculated\ dose - Normalised\ measured\ dose \quad (5)$$

3.1 Findings of the in-vivo phantom measurements

The measurements with the semiconductor detectors showed that the Rectum probe (R)3 and Bladder probe (B) samples with 4% in the mean value showed the lowest deviation from the calculated dose. R5 showed the highest deviation with mean 13.6%, from the individual measurements shown in table 4 it can be seen that this high deviation applied to all Measurement Series (MS).

Table 4: Difference between the calculation of the TPS and the measurements.

Setup	R1 [%]	R2 [%]	R3 [%]	R4 [%]	R5 [%]	B [%]
MS 1	4.4	8.2	8.1	8.2	13.6	-1.2
MS 2	6.0	10.2	7.6	8.7	15.6	-2.9
MS 3	10.1	9.4	2.1	6.6	15.4	-4.6
MS 4	3.5	4.0	-0.2	1.2	9.9	-5.1
Mean	6.0	8.0	4.4	6.2	13.6	-3.5
SD	2.5	2.4	3.5	3.0	2.3	1.5

When comparing the linearity, the figure 13 shows that all detectors had linearity at 2 Gy. The R3 and B samples were so congruent that they covered each other in the graph. It was also observed that fluctuations, as they occurred at 0.5 Gy, were present in all probes, whereby the R5 showed a larger drop here.

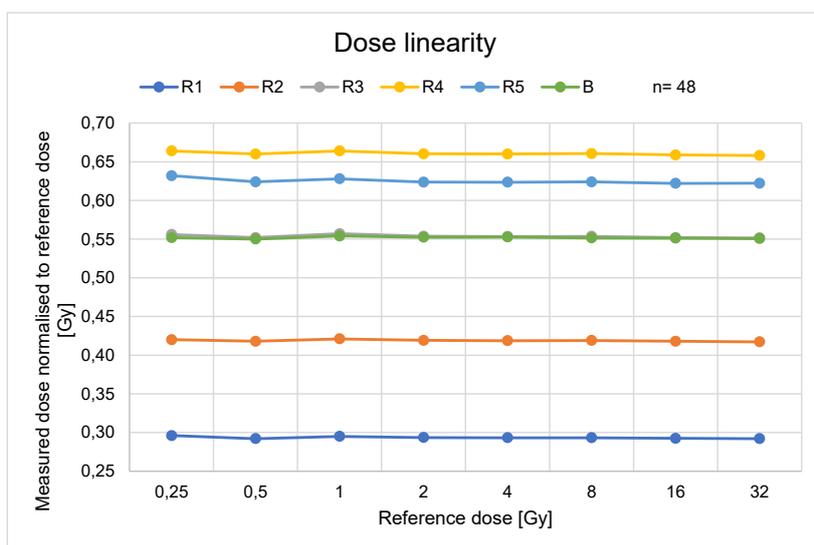


Figure 13: Diagram of the linearity by different doses from the semiconductor detectors. Eight applications were made for the rectal probe and 40 applications was made for the bladder probe. The measured values were normalised to 1 Gy. The abbreviation means Rectum probe (R) and Bladder probe (B).

3.2 Findings of the needle phantom measurements

The following graphs are used to compare the different chambers. The individual data for each detector are presented in tables, where the results for each detector are listed. The value of the max. signal calculated length in the tables was taken from figure 9. Exemplary for some measurements the detailed data are attached to the appendix.

3.2.1 Dose linearity of "point-source" irradiation

The detectors shown in the figure 14 a linear behaviour from 100 s onwards. Between 40 and 100 s there was a continuous slight decrease, before that the highest fluctuation occurred. The detectors all showed the same behaviour. Figure 15 shows, that the linearity was given for all detectors except the microDiamond from the beginning of the measurement. The microDiamond shows a slight decrease in a range from 10 to 50 s.

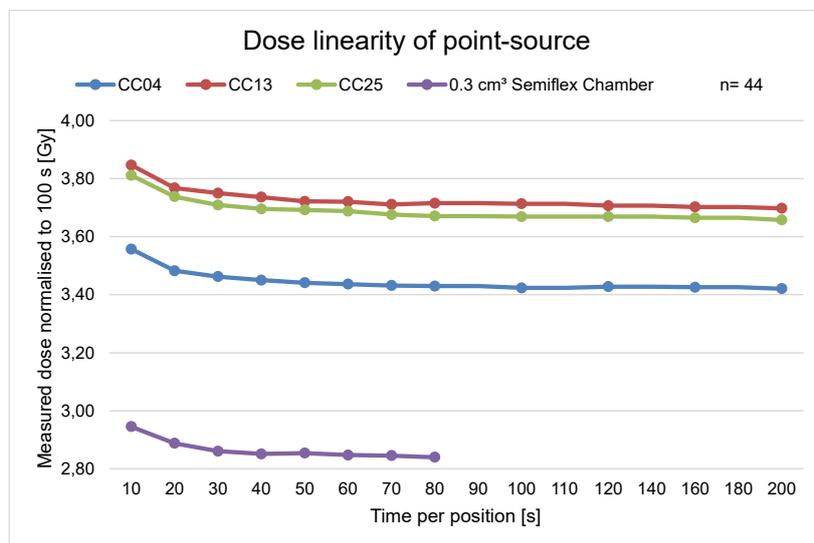


Figure 14: Diagram showing the linearity of different radiation times from all used detectors. The point dose was set for every detector individual and was placed at his max. signal high.

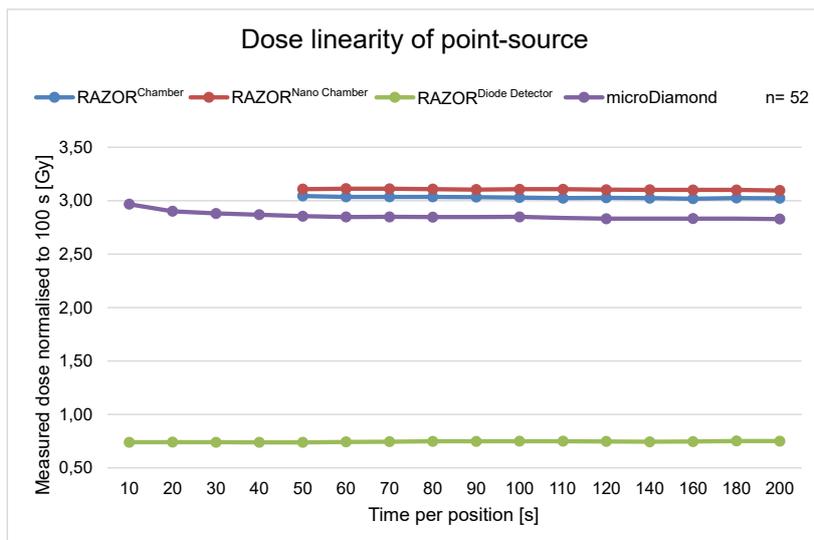


Figure 15: Diagram showing the linear of different radiation times for all used detectors. The point dose was set for every detector individual and was placed at his max. signal high.

3.2.2 Different "active lengths" irradiation

The irradiation of different lengths showed that the detectors CC04, CC25, RAZOR^{Diode Detector} and microDiamond had a highest deviation of $\pm 1\%$. The 0.3 cm^3 Semiflex Chamber showed a barely noticeable smaller variation of -1.5% . The detectors CC13 and RAZOR^{Chamber} had a variation of $\pm 3\%$. With -6% the RAZOR^{Nano Chamber} had the highest difference to the TPS. From the figure 16 and 17 it could be seen that an increase of the irradiation length achieved a better agreement to the TPS. The improvement was different for each detector.

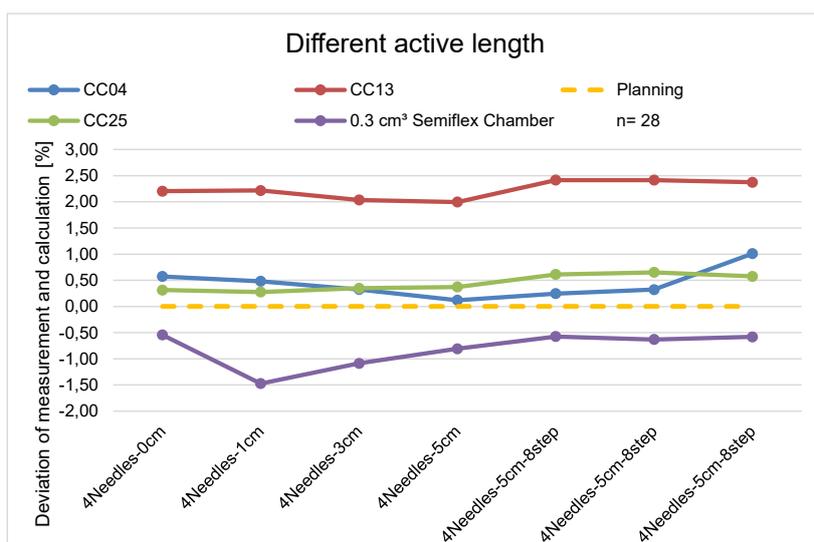


Figure 16: Diagram showing the deviations between calculated dose by the TPS (0%) and measured for the CC's and the 0.3 cm^3 Semiflex Chamber. The point dose (4Needles-0cm) was set for detector individually and was placed at the max. signal high. The last three values (4Needles-5cm-8step) were the same.

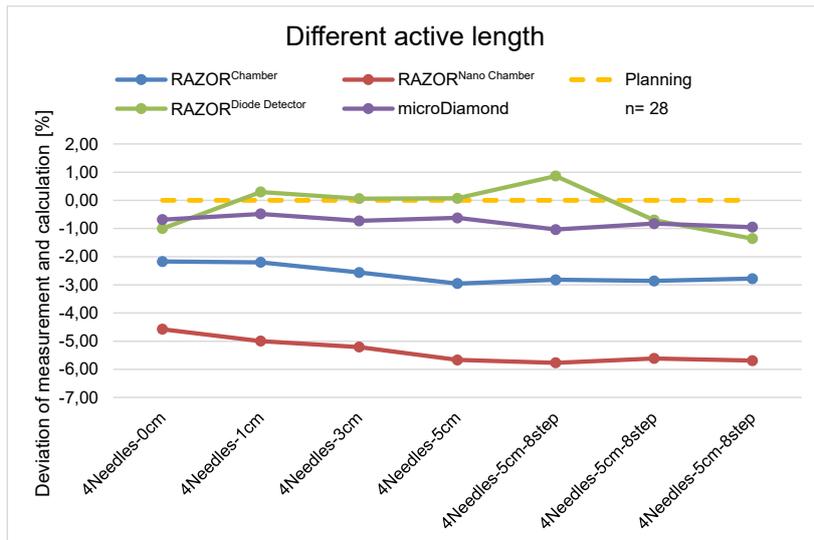


Figure 17: Diagram showing the deviations between calculated dose by the TPS (0%) and measured doses for the RAZOR's and the microDiamond detector. The point dose (4Needles-0cm) was set for every detector individual and was placed at his max. Signal high. The last three values (4Needles-5cm-8step) were the same.

3.2.3 Comparative measurements of all detectors on one day irradiation

In the direct comparison of all detectors for "point irradiation" (figure 18) and "active length" (figure 19), all detectors showed the same behaviour. The exception is RAZOR^{Diode Detector} which showed a higher deviation from the treatment planning at the 5 cm "active length". The detectors RAZOR^{Chamber} and RAZOR^{Nano Chamber} showed the highest difference to the calculated dose for both measurement variants.

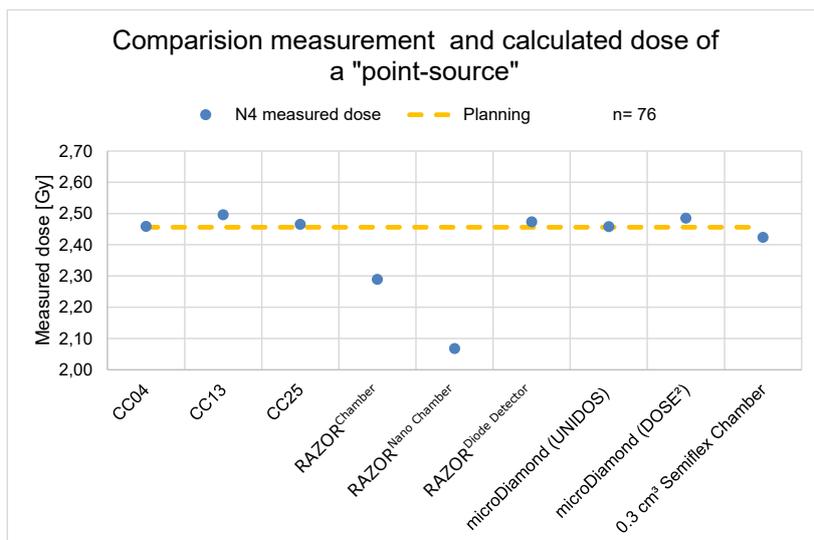


Figure 18: Diagram showing the deviations between calculated dose by the TPS and measured doses of a "point source" for the different detectors. The abbreviation mean Needle number (N).

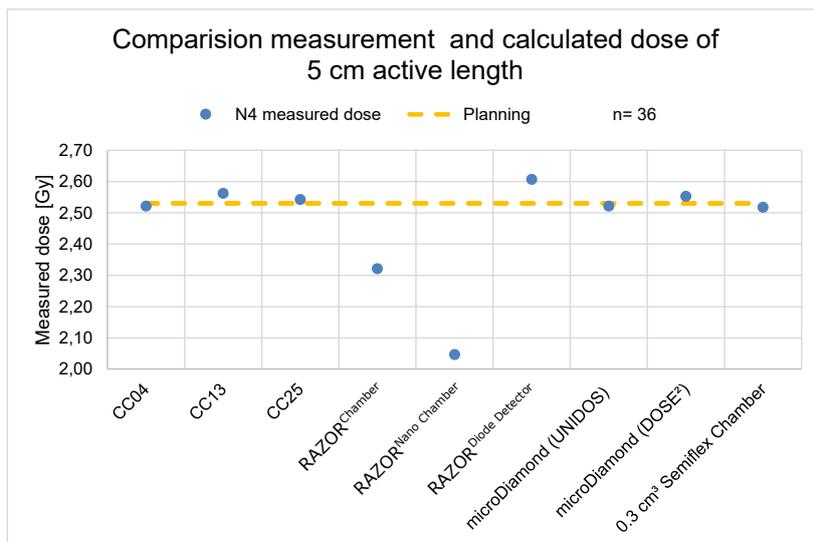


Figure 19: Diagram showing the deviations between calculated dose by the TPS and measured doses for the different detectors. The abbreviation mean Needle number (N).

3.2.4 Comparative of 2 and 4 needle irradiation

The direct comparison of the different measurement methods with 2 and 4 needles for the CC04 and CC25 showed the best agreement for measurement one and two. In figure 20 it could be seen that the CC13 always has an 1% offset.

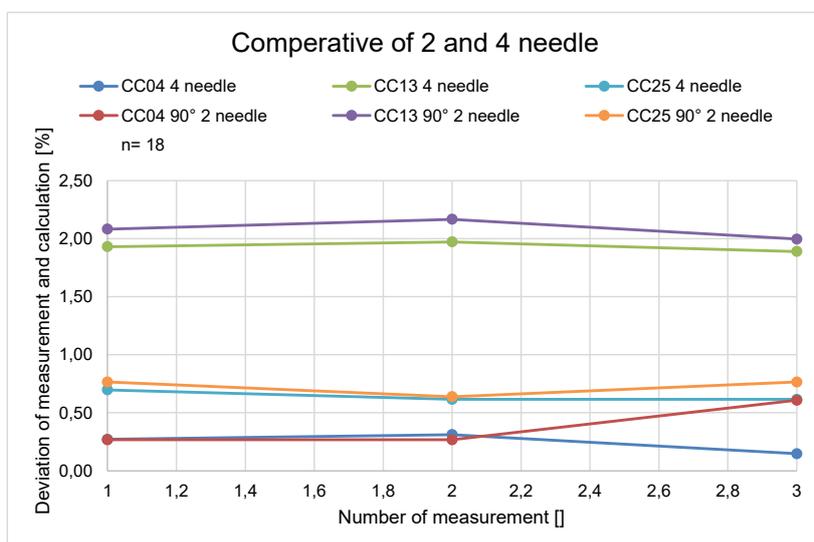


Figure 20: Diagram showing the deviations between the two possibilities using from the needle phantom.

3.2.5 Overview of all detectors

The CC04 (table 5) showed the smallest deviation between calculations of the treatment planning and the measurements for a "point-source". The dose linearity of "point-source" showed with mean 5.93 % the highest deviation for all measurements made with the CC04. Here it must be noted that the deviation of normalised data for this measurement was mean 0.24 %.

Table 5: Summary of all results for the measurements with the CC04 in the needle phantom.

CC04			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1110 ± 1	1110 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	5.93	-0.24
	SD	1.13	1.07
	Min.	5.06	-3.38
	Max.	9.25	0.59
Different active lengths	Mean	0.44	
	SD	0.27	
	Min.	0.12	
	Max.	1.01	
Comparative measurements of all detectors an one day	Point-source	0.11	
	Active length	-0.35	
		Deviation 4 needle [%]	Deviation Phantom 90° 2 needle [%]
Comparative of 2 and 4 needle	Mean	0.24	0.38
	SD	0.07	0.16
	Min.	0.15	0.27
	Max.	0.31	0.61

The CC13 (table 6) detector showed the lowest deviation in the comparative measurements with the "active-length". When comparing the measurement results it can be seen that with mean 2.43% the Dose linearity of "point-source" had the highest deviation between measured and calculated dose. The deviation of normalised data for this measurement was mean 0.29%.

Table 6: Summary of all results for the measurements with the CC13 in the needle phantom.

CC13			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1111 ± 1	1112 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	2.43	-0.29
	SD	1.09	1.06
	Min.	1.47	-3.37
	Max.	5.57	0.64
Different active lengths	Mean	2.24	
	SD	0.16	
	Min.	2.00	
	Max.	2.42	
Comparative measurements of all detectors an one day	Point-source	1.62	
	Active length	1.26	
		Deviation 4 needle [%]	Deviation Phantom 90° 2 needle [%]
Comparative of 2 and 4 needle	Mean	1.93	2.08
	SD	0.03	0.07
	Min.	1.89	2.00
	Max.	1.97	2.17

The comparison of all the measurement results for the CC25 (table 7) chamber showed that the comparative measurements with "point-source" had the smallest deviation. Again, the dose linearity of "point-source" showed the largest difference to the calculated dose.

Table 7: Summary of all results for the measurements with the CC25 in the needle phantom.

CC25			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1113 ± 1	1113 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	1.40	-0.08
	SD	1.13	1.11
	Min.	0.38	-3.23
	Max.	4.59	0.93
Different active lengths	Mean	0.45	
	SD	0.15	
	Min.	0.28	
	Max.	0.65	
Comparative measurements of all detectors an one day	Point-source	0.38	
	Active length	0.49	
		Deviation 4 needle [%]	Deviation Phantom 90° 2 needle [%]
Comparative of 2 and 4 needle	Mean	0.64	0.72
	SD	0.04	0.06
	Min.	0.62	0.64
	Max.	0.70	0.77

The evaluation for the RAZOR^{Chamber} (table 8) showed that the dose linearity of "point-source" had the lowest real deviation from design compared to the other measurements for this chamber. With mean 8.26 % the comparative measurements with "active length" had the highest difference.

The RAZOR^{Nano Chamber} (table 9) showed with mean 19.14 % deviation for the comparative measurements with "active length", the highest achieved deviation between measured and calculated dose of all detectors used. The dose linearity of "point-source" corresponded with deviation between measured and calculated dose of mean 3.72 % to the measurements with the lowest deviation for this chamber.

Table 8: Summary of all results for the measurements with the RAZOR^{Chamber} in the needle phantom.

RAZOR ^{Chamber}			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1112 ± 1	1112 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	-0.61	0.48
	SD	0.23	0.23
	Min.	-0.97	0.00
	Max.	-0.13	0.84
Different active lengths	Mean	-2.62	
	SD	0.30	
	Min.	-2.96	
	Max.	-2.17	
Comparative measurements of all detectors an one day	Point-source	-6.79	
	Active length	-8.26	

Table 9: Summary of all results for the measurements with the RAZOR^{Nano Chamber} in the needle phantom.

RAZOR ^{Nano Chamber}			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1113 ± 1	1113 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	-3.72	0.12
	SD	0.15	0.16
	Min.	-4.03	-0.11
	Max.	-3.50	0.44
Different active lengths	Mean	-5.36	
	SD	0.41	
	Min.	-5.77	
	Max.	-4.58	
Comparative measurements of all detectors an one day	Point-source	-15.81	
	Active length	-19.14	

The explanation of the following two tables is given on the next page 28.

Table 10: Summary of all results for the measurements with the RAZOR^{Diode Detector} in the needle phantom.

RAZOR ^{Diode Detector}			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1104 ± 1	1101 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	-0.32	-0.84
	SD	0.58	0.59
	Min.	-1.16	-1.68
	Max.	0.51	0.01
Different active lengths	Mean	-0.25	
	SD	0.73	
	Min.	-1.36	
	Max.	0.86	
Comparative measurements of all detectors an one day	Point-source	0.71	
	Active length	3.03	

Table 11: Summary of all results for the measurements with the 0.3 cm³ Semiflex Chamber in the needle phantom.

0.3 cm ³ Semiflex Chamber			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1107 ± 1	1106 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	0.40	-0.44
	SD	1.15	1.15
	Min.	-0.53	-3.20
	Max.	3.16	0.49
Different active lengths	Mean	-0.81	
	SD	0.32	
	Min.	-1.47	
	Max.	-0.54	
Comparative measurements of all detectors an one day	Point-source	-1.31	
	Active length	-0.47	

In the treatment of different "active lengths", the RAZOR^{Diode Detector} (table 10) reached the lowest deviation of all detectors with mean 0.25 %. The evaluation further showed that the comparative measurements by "active length" showed the highest deviation. The measurement of the max. signal had a difference of 3 mm when comparing measurements and the drawing.

The Semiflex Chamber (table 11) had the smallest deviation to the calculated dose with mean 0.40 % for the dose linearity of "point-source", compared to the other treatments. However the highest deviation between measured and calculated dose of mean 1.31 % for the comparative measurement with "point-source".

The microDiamond (table 12) had the lowest deviation of all chambers with mean 0.09 % for comparative measurements with "point-source" by using the Unidos electrometer. The highest difference to the treatment planning had the comparative measurements at "point-source" with the Dose².

Table 12: Summary of all results for the measurements with the microDiamond in the needle phantom.

microDiamond			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1104 ± 1	1103 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	0.31	-0.27
	SD	1.31	1.31
	Min.	-0.92	-3.94
	Max.	3.97	0.95
Different active lengths	Mean	-0.76	
	SD	0.18	
	Min.	-1.04	
	Max.	-0.48	
Comparative measurements of all detectors an one day	Point-source (Unidos)	0.09	
	Active length (Unidos)	-0.35	
	Point-source (Dose ²)	1.19	
	Active length (Dose ²)	0.90	

3.3 Findings of the water phantom measurements

The following graphs are used to compare the different chambers. The individual data for each detector are presented in tables, where the results for each detector are listed. The value of the max. signal calculated length in the tables was taken from figure 12. Exemplary for some measurements the detailed data are attached to the appendix.

3.3.1 Dose linearity of "point-source" irradiation

Figure 21 showed that all detectors had a linear behaviour during this measurement. But there were three distinctive spots. In the case of the RAZOR^{Chamber}, a drop occurred at 160 s, which then returned to a linear pattern. The CC25 dropped continuously from 10 to 30 s continuously before it showed linearity. The RAZOR^{Nano Chamber} exhibited a short deviation of linearity in the range of 20 s.

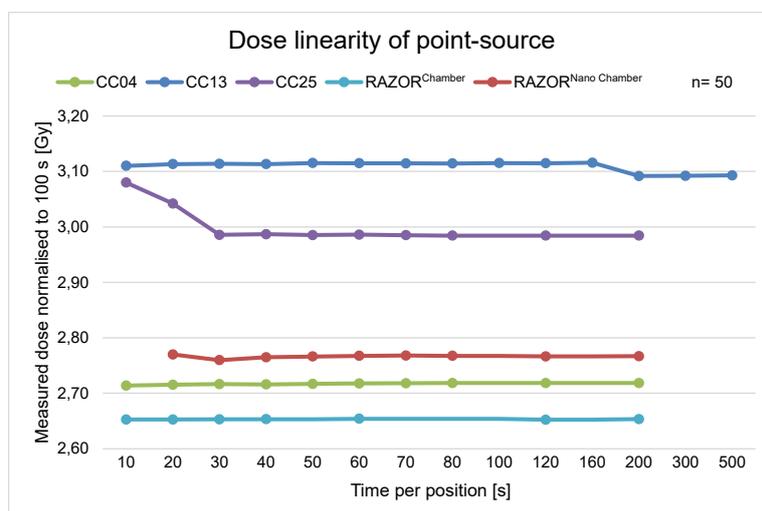


Figure 21: Diagram showing the linearity of different radiation times from all used detectors. The point dose was set for every detector individual and was placed at his max. signal high. The measurement was normalised at 100 s.

3.3.2 "Point-source" - depth dose irradiation

For the "point-source" depth dose, all chambers showed a high level of agreement with the treatment planning, as shown in figure 22. Only the values at 15 mm show a higher variation with CC25 showing the highest difference.

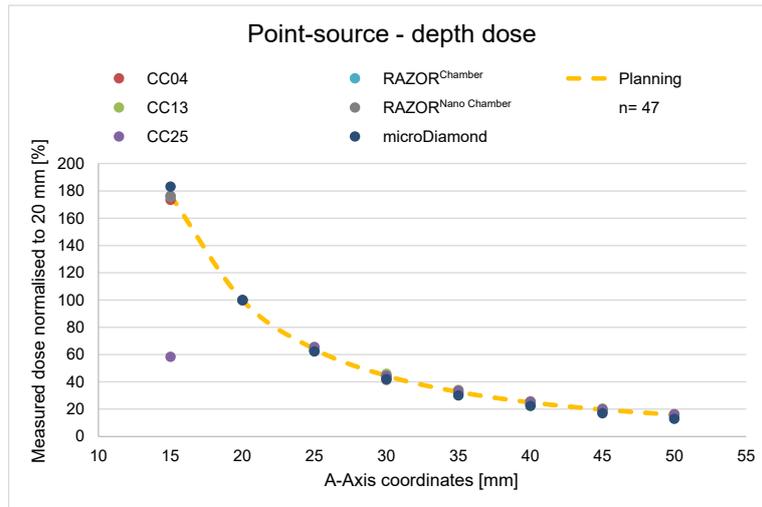


Figure 22: Diagram showing the deviations between calculated dose by the TPS and measured doses for the different detectors. The different A-axis coordinates represent the depth dose. The point dose was set for every detector individual and was placed at his max. Signal high. The measurement was normalised at 20 mm.

3.3.3 "Point-source" - cross profile irradiation

The measurements of the microDiamond and the CC25 chamber showed in figures 23 and 25 that with increasing distance of the A-axis the percentage deviation from the calculated to expected measurement result decreased more and more. The highest deviation was always in the range of 0 mm of the A-axis. The CC13 showed in its figure 24 that the distance of the A-axis caused a not so large change of the treatment planning difference. Whereby the positive deflection at 20 mm was the best match with the calculated dose.

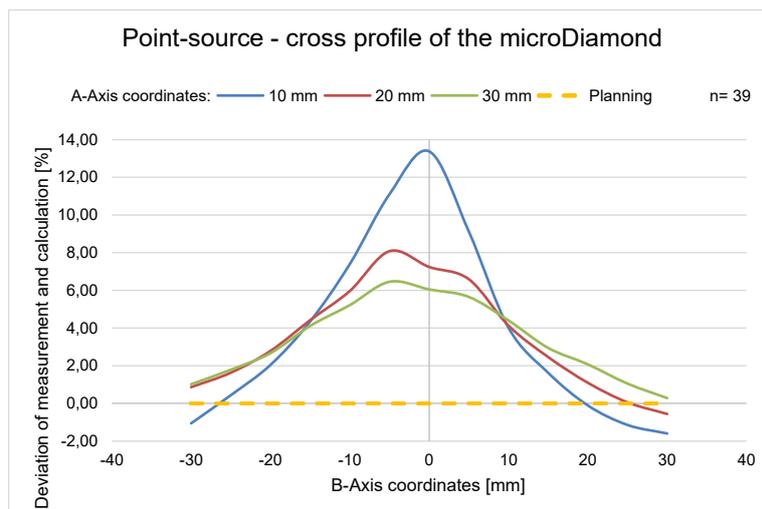


Figure 23: Diagram showing the deviation between the different Axis-coordinates A and B for the microDiamond. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile. The point dose was set at his max. Signal high.

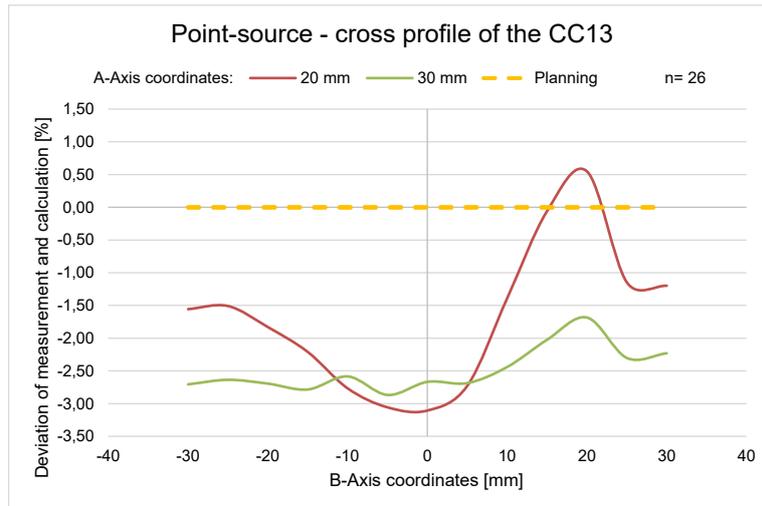


Figure 24: Diagram showing the deviation between the different Axis-coordinates A and B for the CC13. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile. The point dose was set at his max. Signal high.

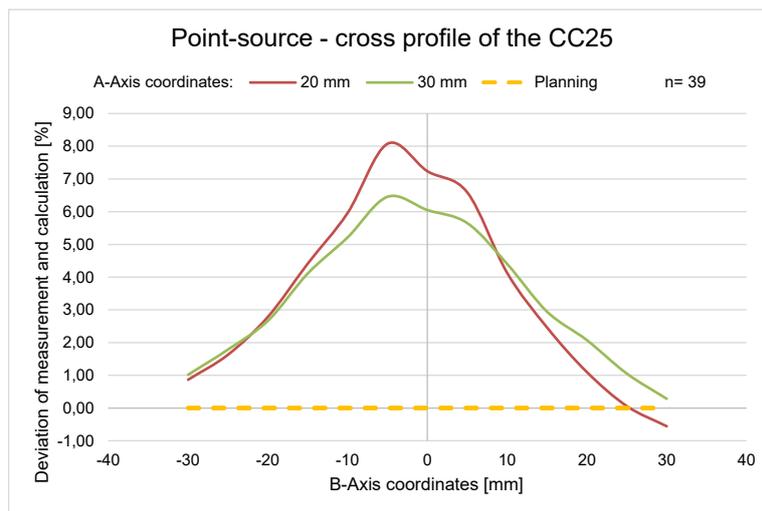


Figure 25: Diagram showing the deviation between the different Axis-coordinates A and B for the CC25. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile. The point dose was set at his max. Signal high.

3.3.4 "Active length" - depth dose irradiation

In these measurement tests, the CC04 and the CC13 showed the smallest deviation with 3 % variation around the design. With 6 %, the CC25 and RAZOR^{Nano Chamber} were those with the highest deviation from the expected calculated measured value. Figures 26 and 27 did not show that the accuracy of the measurements would increase with an increase in the "active length".

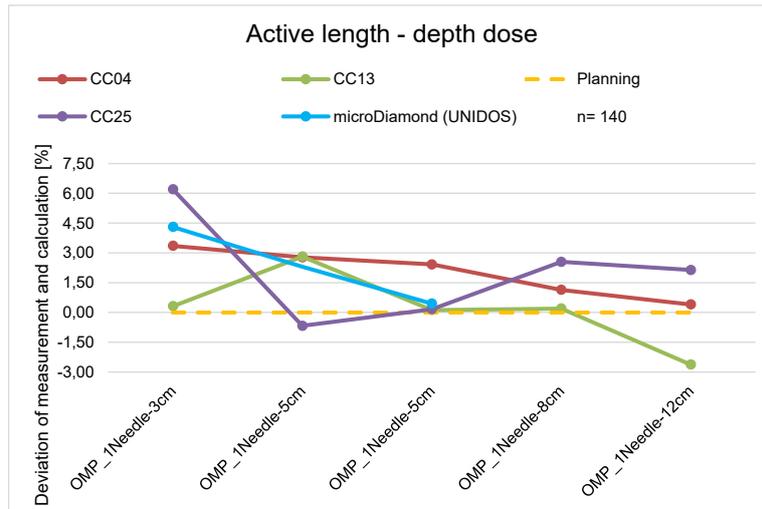


Figure 26: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses. The active length was set for every detector individual and rise up form three to twelve mm.

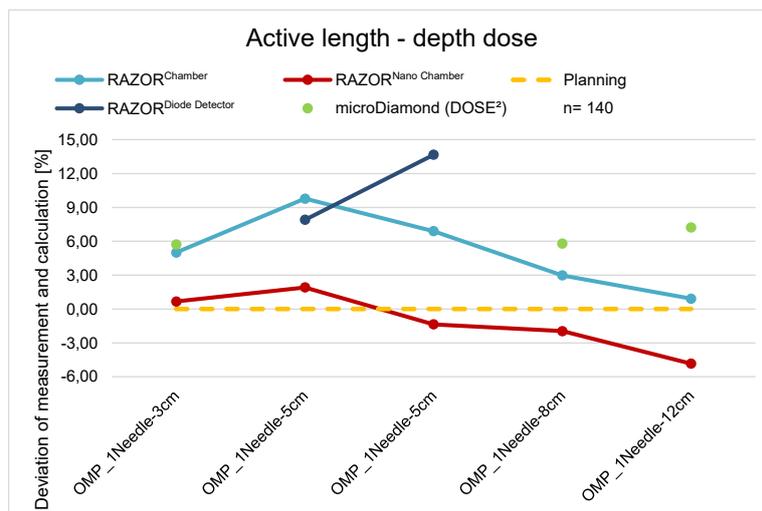


Figure 27: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses. The "active length" was set for every detector individual and rise up form three to twelve mm.

3.3.5 "Active length" - cross profile irradiation

When evaluating the figure 28 it became obvious that with an "active length" of 3 cm the CC13 showed the smallest difference to the treatment planning. The microDiamond had its smallest deviation at an A-axis distance of 20 mm. At an irradiation length of 5 cm, see figures 29 and 30, the microDiamond the CC04 and CC25 showed the highest deviation at a B-axis of -10 to 10 mm. Increasing the A-axis again contributed to a convergence to treatment planning. The CC13 showed the best agreement with the calculated dose, whereby an increase in the distance in the A-axis no longer provided a large improvement. With an "active length" of 8 cm,

CC13 was closest to the calculated dose, the microDiamond varied most in the B-axis range from -50 to 50 mm. Also again, see figure 31, that the higher distance to the needle (higher A-axis) provided an improvement in the knife edge. Figure 32 showed a consistent deviation to the design for both detectors used.

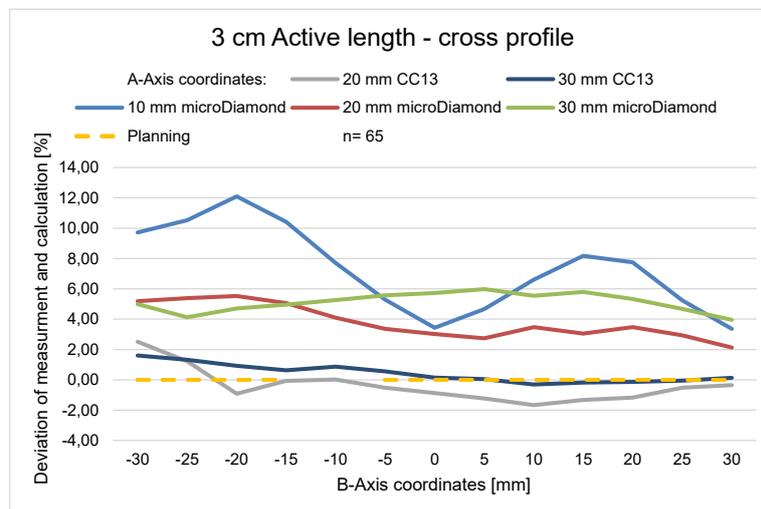


Figure 28: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses when the A- and B-Axis coordinates rise up. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile.

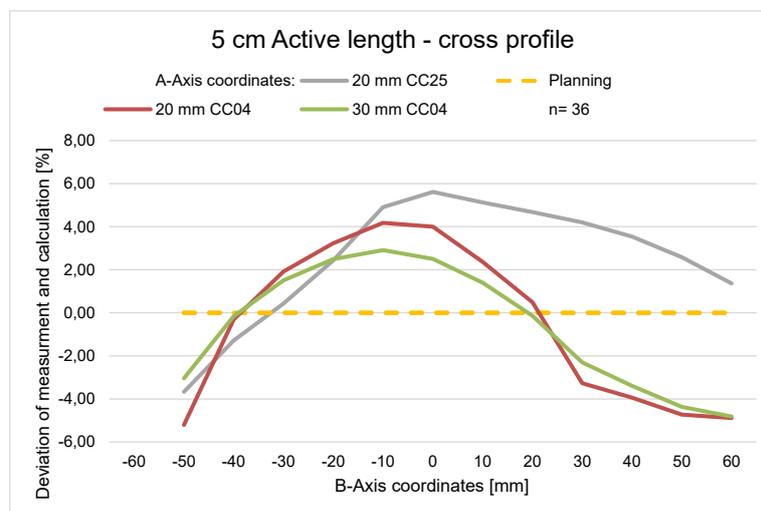


Figure 29: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses when the A- and B-Axis coordinates rise up. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile.

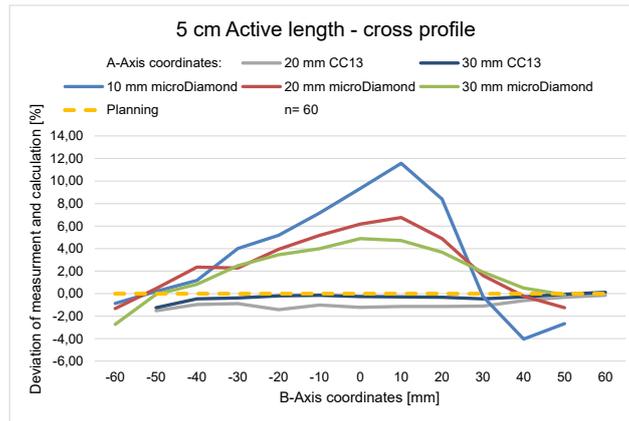


Figure 30: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses when the A- and B-Axis coordinates rise up. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile.

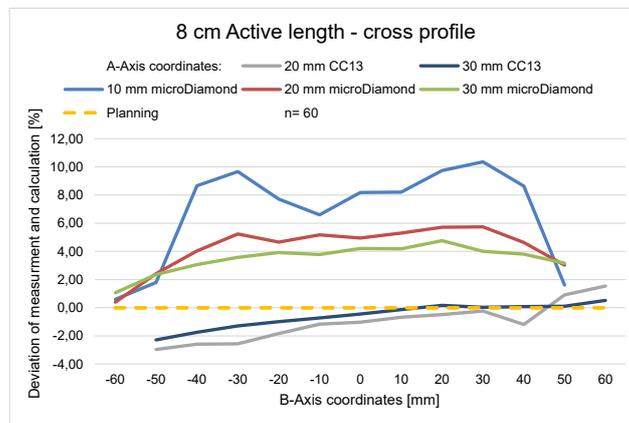


Figure 31: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses when the A- and B-Axis coordinates rise up. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile.

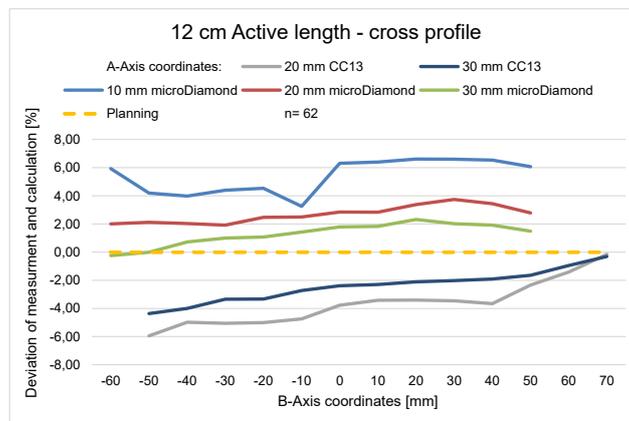


Figure 32: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses when the A- and B-Axis coordinates rise up. The different A-axis coordinates represent the depth dose. The B-axis represent the variation of the detector in the cross profile.

3.3.6 5 needles in triangular configuration irradiation

For the 5 needles in triangular configuration (see figure 33), the best match to calculated dose was achieved with the CC25 at a C-axis spacing of 8 mm. The measurements showed that all the chambers used had the same measurement curve, and were only offset by a few percent. Furthermore, a higher C-axis distance did not lead to noticeably better measurement results.

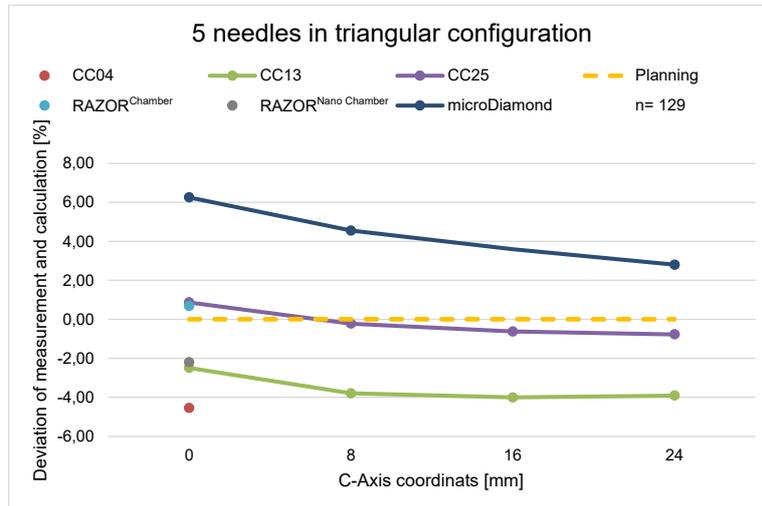


Figure 33: Diagram showing the deviations between calculated dose by the TPS (0,%) and measured doses when the C-Axis coordinate rise up from zero to twenty-four mm. The different C-axis coordinates represent the movement in horizontal direction.

3.3.7 Dependence on water heights irradiation

The CC13 showed a decrease in dose at a water height of 2.5 cm. The RAZOR^{Nano} Chamber showed the decrease from 2.0 cm. Both chambers showed, as can be seen in figure 34, an increasing decrease of the dose with decreasing water height.

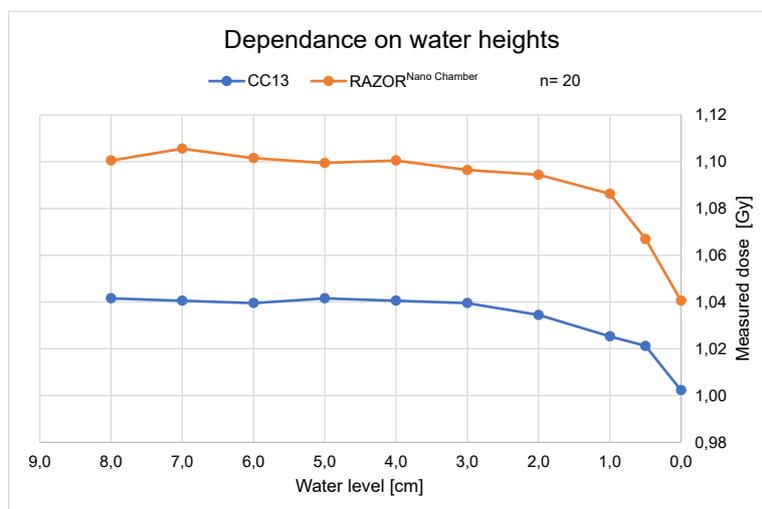


Figure 34: Diagram showing the measured dose by different water level.

3.3.8 Overview of all detectors

The CC04 (table 13) showed the lowest deviation from all measurements made with this chamber in the "active length" cross profile with mean 0.57%. The 5 needles in triangular configuration had the highest deviation from treatment planning. When looking at the deviation of normalised data, it was noticeable that all measured values were below 1.5% related to the mean values. The measurement with the lowest deviation was the dose linearity of point-source with mean 0.02%. The highest value for the "active length" of cross profile was mean 1.22%.

Table 13: Summary of all results for the measurements setups with the CC04 in the water phantom.

CC04			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1132 ± 1	1130 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	2.29	0.02
	SD	0.06	0.05
	Min.	2.17	-0.03
	Max.	2.34	0.14
Point-source - depth dose	Mean	3.27	0.85
	SD	0.95	1.07
	Min.	1.95	0.00
	Max.	5.04	3.63
Active length - depth dose	Mean	2.12	0.65
	SD	1.36	0.87
	Min.	-0.53	-0.43
	Max.	4.93	3.31
Active length - cross profile	Mean	-0.57	1.22
	SD	3.15	1.68
	Min.	-5.21	-4.89
	Max.	4.18	3.88
5 needles in triangular configuration	Mean	-4.55	1.13
	SD	6.78	0.84
	Min.	-19.64	-0.05
	Max.	2.00	2.56

The CC13 (table 14) achieved its best result for the "active length" in the depth dose. The 5 needles in triangular configuration showed the largest difference to the calculated dose with mean -3.55%. The deviation of normalised data of this chamber showed the lowest difference of mean -0.05% for the "active length" by cross profile. With mean -0.85%, the "point-source"

depth dose was furthest away from the normalised values. Nevertheless, all deviations of normalised data were below 1 % related to the mean values. The measurement of max. signal showed a difference of 4 mm for the CC13 when comparing measurements and the drawing.

Table 14: Summary of all results for the measurements setups with the CC13 in the water phantom.

CC13			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1132 ± 1	1128 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	-2.10	0.17
	SD	0.29	0.29
	Min.	-2.66	-0.03
	Max.	-1.91	0.74
Point-source - depth dose	Mean	0.57	-0.85
	SD	1.52	0.50
	Min.	-2.24	-1.54
	Max.	2.36	0.00
Point-source - cross profile	Mean	-2.09	-0.43
	SD	0.88	0.55
	Min.	-3.11	-1.97
	Max.	0.55	0.20
Active length - depth dose	Mean	0.15	0.10
	SD	2.15	1.25
	Min.	-6.36	-1.78
	Max.	3.42	4.51
Active length - cross profile	Mean	-1.13	-0.05
	SD	1.59	0.74
	Min.	-5.96	-3.89
	Max.	2.51	1.74
5 needles in triangular configuration	Mean	-3.55	-0.58
	SD	2.06	1.54
	Min.	-8.65	-2.06
	Max.	-0.78	4.07
		MS [Gy]	
Dependance on water heights	Mean	1.033	
	SD	0.012	
	Min.	1.002	
	Max.	1.042	

The CC25 (table 15) showed the most ideal match to the treatment planning with mean -0.05 % for the 5 needles in triangular configuration. For the dose linearity of "point-source" it was mean 6.68 % with an deviation of normalised data of mean -0.48 %. The "point-source" cross profile and 5 needles in triangular configuration with mean 0.33 % each were the measurements with the lowest deviations of normalised data. The "active length" cross profile measurement showed the highest deviation of normalised data with mean 0.89 %, whereby the chamber always showed an deviation of normalised data of < 1 % related to the mean values.

Table 15: Summary of all results for the measurements setups with the CC25 in the water phantom.

CC25			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1129 ± 1	1127 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	6.68	-0.48
	SD	1.12	1.05
	Min.	6.11	-3.14
	Max.	9.51	0.06
Point-source - depth dose	Mean	5.40	-0.38
	SD	1.27	0.58
	Min.	3.15	-1.56
	Max.	6.75	0.55
Point-source - cross profile	Mean	5.21	-0.33
	SD	1.89	0.75
	Min.	2.72	-2.02
	Max.	8.90	0.74
Active length - depth dose	Mean	1.44	0.85
	SD	4.24	0.88
	Min.	-12.75	-0.83
	Max.	7.21	2.96
Active length - cross profile	Mean	2.49	0.89
	SD	2.73	1.45
	Min.	-3.67	-2.89
	Max.	5.62	2.83
5 needles in triangular configuration	Mean	-0.05	0.33
	SD	0.93	0.82
	Min.	-2.18	-0.23
	Max.	1.31	2.52

The RAZOR^{Chamber} (table 16) had its highest difference to the calculated dose for the "point-source" - depth dose, but the 5 needles in triangular configuration was at least mean 0.68%. The deviations of normalised data were mean 0.04% for the dose linearity of point-source measurement and mean 1.42% for "active length" depth dose. It was found that the deviations of normalised data were always below 1.5% related to the mean values for this chamber.

Table 16: Summary of all results for the measurements setups with the RAZOR^{Chamber} in the water phantom.

RAZOR ^{Chamber}			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1129 ± 1	1128 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	6.54	0.04
	SD	0.02	0.02
	Min.	6.51	0.00
	Max.	6.58	0.06
Point-source - depth dose	Mean	6.68	0.60
	SD	1.47	0.28
	Min.	4.11	0.00
	Max.	9.00	1.06
Active length - depth dose	Mean	5.72	1.42
	SD	3.92	2.25
	Min.	-2.13	0.00
	Max.	11.02	15.99
5 needles in triangular configuration	Mean	0.68	0.65
	SD	1.72	0.52
	Min.	-2.35	-0.37
	Max.	2.89	1.21

For the RAZOR^{Nano Chamber} (table 17), the measurements of the dose linearity of "point-source", showed the highest deviation to the treatment planning with mean 5.25 %. The "active length" by depth dose measurements showed the smallest difference for this chamber with mean - 0.72 %. The comparison of the deviation of normalised data showed that the dose linearity of "point-source" had the lowest value with mean 0.04 %. With mean 1.57 %, the measurements of the "point-source" depth dose was the highest in summary. This chamber achieved deviations of normalised data of less than 2 % related to the mean values.

Table 17: Summary of all results for the measurements setups with the RAZOR^{Nano Chamber} in the water phantom.

RAZOR ^{Nano Chamber}			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1129 ± 1	1127 ± 1
		Deviation [%]	Deviation of normalised data [%]
Dose linearity of point-source	Mean	5.25	0.04
	SD	0.10	0.10
	Min.	5.00	-0.09
	Max.	5.39	0.28
Point-source - depth dose	Mean	1.91	1.57
	SD	4.15	0.87
	Min.	-4.23	0.00
	Max.	7.73	3.12
Active length - depth dose	Mean	-0.72	1.28
	SD	3.89	1.01
	Min.	-10.57	-0.66
	Max.	4.97	2.98
5 needles in triangular configuration	Mean	-2.20	1.50
	SD	3.37	0.86
	Min.	-7.85	0.00
	Max.	1.92	2.39
		MS [Gy]	
Dependance on water heights	Mean	1.089	
	SD	0.019	
	Min.	1.041	
	Max.	1.106	

For the RAZOR^{Diode Detector} (table 18) one measurement setup was looked at. It is visible that the deviation for the "active length" at depth-dose was mean 10.3 % with an deviation of normalised data of mean -0.22 %.

Table 18: Summary of all results for the measurements setups with the RAZOR^{Diode Detector} in the water phantom.

RAZOR ^{Diode Detector}			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1119 ± 1	1118 ± 1
		Deviation [%]	Deviation of normalised data [%]
Active length - depth dose	Mean	10.30	-0.22
	SD	4.78	4.88
	Min.	4.13	-7.63
	Max.	23.59	16.24

In the case of the microDiamond (table 19), the measurements were carried out with different electrometers. The comparison of the measurements showed that for both the Unidos and the Dose² the highest deviation was found in the "point-source" depth dose measurements. No systematic difference for the Unidos and Dose² electrometer could be found.

The microDiamond in combination with the Unidos showed the best agreement to the calculated dose for the "active length" depth dose. For the Dose², the measurements of the "active length" at cross profile with mean 3.70 % was the measurement that showed the smallest difference to the calculated dose.

When comparing the deviations of normalised data, for the microDiamond with both electrometers, the lowest measured values were mean -1.25 % (Unidos) and mean 0.62 % (Dose²). For the "active length" depth dose, the detector for the measurements with the Unidos achieved the highest deviation of normalised data of mean 1.86 %.

The combination of microDiamond and Dose² achieved the most striking difference of mean -32.90 % for the "point-source" depth dose. This high deviation resulted from the fact that the microDiamond was at a distance of 5 mm from the source. As a result, the detector received more dose than was actually planned.

The measured deviations of normalised data were in a value range of less than 5 % related to the mean values.

Table 19: Summary of all results for the measurements setups with the microDiamond in the water phantom.

microDiamond			
Treatment	Parameter	Length measured [mm]	Length calculated (from figure) [mm]
Distance for the max. Signal		1119 ± 1	1118 ± 1
		Deviation [%]	Deviation of normalised data [%]
Point-source - depth dose	Mean (Unidos)	8.55	
	SD (Unidos)	4.66	
	Min. (Unidos)	3.95	
	Max. (Unidos)	17.63	
	Mean (Dose ²)	8.89	-32.90
	SD (Dose ²)	7.41	90.59
	Min. (Dose ²)	3.71	-303.66
	Max. (Dose ²)	28.87	0.99
Point-source - cross profile	Mean	3.54	1.41
	SD	3.40	0.93
	Min.	-1.60	-0.70
	Max.	13.38	4.02
Active length - depth dose	Mean (Unidos)	2.37	-1.86
	SD (Unidos)	2.25	4.98
	Min. (Unidos)	-0.40	-18.25
	Max. (Unidos)	6.80	0.46
	Mean (Dose ²)	6.25	-4.82
	SD (Dose ²)	3.29	13.09
	Min. (Dose ²)	3.41	-51.88
	Max. (Dose ²)	18.55	0.71
Active length - cross profile	Mean (Unidos)	5.55	-1.25
	SD (Unidos)	2.71	1.33
	Min. (Unidos)	2.12	-4.59
	Max. (Unidos)	12.09	0.34
	Mean (Dose ²)	3.70	0.62
	SD (Dose ²)	2.81	0.95
	Min. (Dose ²)	-4.04	-1.96
	Max. (Dose ²)	11.58	3.70
5 needles in triangular configuration	Mean	4.46	-0.96
	SD	1.81	4.35
	Min.	1.83	-23.24
	Max.	12.37	5.42

4 Discussion

Furthermore, the subdivision enables a better comparison of the detectors with regard to their accuracies and advantages. To highlight all these features, the detectors are subdivided into:

- Semiconductor detectors
 - Semiconductor detector T9112 (Rectum)
 - Semiconductor detector T9113 (Bladder)
 - RAZOR^{Diode Detector}
- Ionisation chambers
 - CC04
 - CC13
 - CC25
 - RAZOR^{Chamber}
 - RAZOR^{Nano Chamber}
 - 0.3 cm³ Semiflex Chamber
- Diamond detector
 - microDiamond

4.1 Analysis of the semiconductor detectors results

The semiconductor detectors T9112 and T9113 show higher deviation to the values of the treatment planning. Whereas in the measurement results of the table 4 the Measurement Series (MS) 4 of the rectum probe shows significantly lower deviations. In the case of MS 4, the cables of the rectum and bladder probe were deliberately twisted in the course of the measurement in order to check whether the position of the diode cables had an influence on the sensitivity of the diodes. The positioning of the diode cables does not play a role as can be seen from the data of the measurement, which can be found in the appendix under "A; In-vivo phantom Data". A comparison of the results of an earlier study with the same semiconductor detectors by Waldhäusl et al. confirms this assumption. Here, deviations between the measured dose of the detectors and the calculated dose of the treatment planning were achieved with an average of $4.9 \pm 3\%$ [33].

The linearity of the semiconductor detector's shows a drop at 0.5 Gy as can be seen in figure 13. A close examination of the measured values for exactly that range revealed a variation between the previous (0.25) and subsequent measurement (1) of 0.002 to 0.008 Gy. This deviation is so small that it can be declared as normal measurement fluctuations. Thus, the semiconductor detectors T9112 and T9113 show a linear behaviour.

In the measurements with the RAZOR^{Diode Detector} in particular the direct comparison between the results of the needle phantom (table 10) and the water phantom (table 18) shows, that the detector in the needle phantom achieves the smaller deviations to the calculated dose. For the needle phantom, a value of less than 1 % was measured related to the mean values. This value refers to both the deviation between measured and calculated doses and the deviation of the normalised data. However, for the comparative measurements with "active length", the deviation is about 3.03 % (see table 10).

No reason can be given for the higher deviation of the comparative measurements with "active length". However, it can be assumed that this measurement result is an outlier because the comparative measurements with "point-source" always delivered good results with all two MS. Furthermore, the RAZOR^{Diode Detector} always showed very small deviations from the treatment planning when measuring different "active lengths". To check whether this was an outlier, further measurements should be carried out.

4.2 Analysis of the ionisation chambers results

For measurements in the water phantom, the CC chambers achieved better measurement results than the RAZOR chambers. Depending on the treatment, the deviation for the CC's was about 0.05-6.68 % (see table 15) and for the RAZOR's about 0.68-6.68 % (see table 16). This slightly higher deviation of the RAZOR's corresponds well to a comparable study by Ballester et al. where the existing measured values of a pinpoint chamber (volume 0.015 cm²) using the Monte Carlo method were compared. Maximum deviation of 10 % was calculated there [34].

In terms of deviation of normalised data, all ion chambers show measured values of less than 2 % (see table 13-17). This is in contrast to the results of the needle phantom measurements where all CC's and RAZOR chambers show the lowest deviation from treatment planning, by comparison needle and water phantom.

When comparing the CC's, it is noticeable that the CC04 has performed the worst of all CC's, despite its low volume of 0.04 cm². Moura et al. carried out an investigation with an A1SL (volume 0.053 cm²) that is similar to the dose linearity of "point-source". In the experiment of Moura et al. a mean deviation from treatment planning of 4.81 % was calculated [35].

The CC04 show a deviation of 5.93 % (see table 5) for the linearity of "point-source" measurement. The RAZOR's also show a higher deviation from the calculated dose for the chambers with lower volumes, this can be seen in the graphs 18 and 19. However, this does not affect the deviation of normalised data, which achieves good measurement results for all ion chambers.

The comparison of the linearity of the water phantom (figure 21) and needle phantom (figure 16 and 17) shows that all detectors have a linear behaviour above from a certain irradiation level. Except the microDiamond and the RAZOR^{Diode Detector} these always showed a linear behaviour from the beginning of the measurements. Due to its design and the resulting physical behaviour, the RAZOR^{Diode Detector} does not require any pre-irradiation for the detection of radiation. For the microDiamond and the ionisation chambers, a basic irradiation is recommended/required by the manufacturer (microDiamond). In the case of the diamond, this can be explained by the fact that the traps have to be filled with electrons [27], [20, pp. 89–91], [5, pp. 173–175, 167]. For ionisation chambers it has been observed for a long time that pre-irradiation provides better measurement results. This observation was investigated in detail by McCaffray et al. in a study that identified radiation-induced conductivity as the physical cause necessary pre-irradiation [36]. The deviations at the beginning of the linearity study can be explained by the fact that the CC's basic irradiation was not taken into account, although even some manufacturers refer to it in their operating instructions[22], [23], [21], [24], [25]. This was improved during the study.

In the experiments where "active length" were irradiate, it can be seen that the chambers with small active volume show better agreement to the treatment planning when the "active length" increases. This can be seen in the figures 26 and 27. There is definitely a correlation between "active length" and active volume of the different chambers. This could be due to the higher sensitivity of the small-volume chambers.

In the course of the investigation, it was further noticed that with increasing distance to the source, the agreement with the treatment planning coincided. At a distance of more than 90 mm the deviations began to increase again until 6.04 % at 140 mm (measured with CC25 see appendix C; "Summary depth-dose - Length (3, 5, 8, 12 cm) in the water phantom"). This tendency was also already observed by Vensella et al. and Gromoll et al. [37], [38]. Whereas Vensella applied its distance in the clinically relevant range of 0 to 60 mm and Gromoll measured further up to 180 mm. In the close range of 5 to 15 mm, the microDiamond and the RAZOR^{Diode Detector} achieved deviations of 0.16-18.55 % (see also the appendix C; "Summary depth-dose - Length (3, 5, 8, 12 cm) in the water phantom"), respectively, and were thus significantly worse than the measurements with a distance of more than 15 mm. This is also in line with the investigations of Vensella and Gromoll.

4.3 Analysis of the diamond detector results

When comparing the results of the needle and water phantom for the microDiamond the deviation between measured and calculated dose as well the normalised data in the needle phantom is again less than 1 %, relate to the mean values. For the comparative measurement with "active length" the deviation is mean 1.19% (see table 12). This value may be an outlier, as both the previous measurements of the comparative Measurement with "point-source" and the treatment different "active length" show a much better agreement with the treatment planning. Further measurements with the treatment comparative measurement with "active length" would have been necessary to prove this.

In the measurements with the water phantom, the conformity between measured and calculated dose was not as good as with the needle phantom. This is expressed by the larger difference between both deviations with a value of approximately 10%, related to the mean values (see table 19). This can be explained by the smaller distances between the source and the microDiamond detector.

Laub et al. found that the microDiamond provides very good measurement results for measurements in teletherapy [39]. Based on the measurement results from the study by Laub et al., the microDiamond delivers very good results for the Brachytherapy too. This shows that the microDiamond is also suitable for brachytherapy.

4.4 Conclusion of the investigations

In conclusion, the following essential findings can be summarised from the observed behaviour of the detectors:

- All detectors, with the exception of the semiconductor detectors, require a basic irradiation due to the physical properties of the detectors. Only when this is given, the detectors deliver solid results.
- The type of irradiation "point-source" and "active length" plays an important role for the measurement results. Depending on the chamber used, this fact contributes to the correlation between measured and calculated dose.
- The measurements show a very good agreement with the treatment planning. This applies especially to the clinically relevant dose range of 15 to 50 mm.
- Chambers with a larger active volume achieve for some experimental setups better results on average. This does not mean, however, that chambers with small active volume are

unsuitable. Because of the steep dose gradient this could not been foreseen when starting the measurements. The study shows, that all chambers can be used.

- The measurements with the needle phantom show very good agreement to the results of the TPS. The water phantom shows sometimes higher deviations. The advantage of the needle phantom is the easy and reproducible usage in fixed geometry. The advantage of the much more complex water phantom is, that it offers more possibilities of measuring the dose in each distance.

In summary, it can be said that (1) all detectors used in this study can be used for further dose measurements in brachytherapy. Both, the deviations (mean 0.05 to 10 %) and the deviations of normalised data (mean < 2 %) demonstrate very good measurement results. Special care has to be given to the RAZOR chambers, they should rather be used for deviations measurements and not for deviations of normalised data measurements.

The study shows (2) that the use of the needle phantom enables precise measurements with simultaneous easy handling of the phantom. Since the measurement effort is very manageable with a significant improvement of routinely performed Quality Assurance (QA). Therefore it is also recommended for brachytherapy to include for regular comparative measurement between calculated dose and measured dose in the standard S 5296 [4].

The study also showed, that (3) the verification of TPS measurements with the water phantom provides an additional control that would help to increase safety for the patient and is recommended for commissioning of TPS.

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List of Abbreviations

AAPM	American Association of Physicists in Medicine
B	Bladder probe
CT	Computed Tomography
CV	Coefficient of Variation
DNA	Deoxyribonucleic acid
EC	Electron Capture
HDR	High Dose Rate
MS	Measurement Series
N	Needle number
ND,W	Calibration factor from "Eichstelle" (Dosiemtrielabor Seibersdorf) $N_{D,W}$
OMP	Oncentra Masterplan
PDF	Portable Document Format
PMMA	Polymethylmethacrylat
pTP	Air density correction factor $p_{TP} = k_P$
QA	Quality Assurance
R	Rectum probe
SD	Standard Derivation
TCC	Treatment Communication Console
TCP	Treatment Control Panel
TDU	Treatment Delivery Unit
TPS	Treatment Planning System

Appendices

A In-vivo phantom Data

Table 20: Overview about the different project procedure for the in-vivo phantom. The values in the table stand for the measurement days, the year was omitted.

Treatment	Semiconductor detector T9112 (Rectum)	Semiconductor detector T9113 (Bladder)
Measurements	14.01. 15.01.	14.01. 15.01.
Dose linearity	15.01.	15.01.
Number of measurements(n)	20	20

Summary of the results measurements in the in-vivo phantom

Treatment plan		Ion chamber		Electrometer	
OMP Plan	OMP_Daniela_14.01.2021	Manufacturer	PTW	Manufacturer	PTW
TCC Plan	Daniela HDR	Model	Semiconductor detectors bladder	Model	VIVODOS
Phantom	In-vivo	SN	001291	SN	000327
Source calibration data		Manufacturer	PTW		
Date	28.10.2020	Model	Semiconductor detectors rectum		
Activity [Ci]	12.89	SN	002360		
SN	NLF01D85E5606				

PTW-fn = PTW-File name
R = Rectum probe
B = Bladder probe
SD = Standard deviation

Measurement Series 1							
PTW-fn	Probe set	R1 [Gy]	R2 [Gy]	R3 [Gy]	R4 [Gy]	R5 [Gy]	B [Gy]
Daniela-B_1	B	0.557	0.830	1.174	1.343	1.231	1.143
Daniela-B_2	B	0.556	0.829	1.171	1.340	1.229	1.145
Daniela-B_3	B	0.556	0.829	1.171	1.337	1.224	1.144
Mean		0.556	0.829	1.172	1.340	1.228	1.144
SD		0.0005	0.0005	0.0014	0.0024	0.0029	0.0008

Date	14.01.2021
Source activity [Ci]	6.19
Total treatment time [s]	256
Method	Timed continuous
Range	-
Length [mm]	1270 - 1300

Measurement Series 4							
PTW-fn	Probe set	R1 [Gy]	R2 [Gy]	R3 [Gy]	R4 [Gy]	R5 [Gy]	B [Gy]
Daniela-B_10	B	0.586	0.837	1.105	1.319	1.247	1.104
Daniela-B_11	B	0.557	0.808	1.080	1.243	1.204	1.085
Daniela-B_12	B	0.542	0.783	1.067	1.214	1.129	1.089
Daniela-B_13	B	0.532	0.775	1.095	1.274	1.232	1.076
Daniela-B_14	B	0.541	0.783	1.064	1.221	1.124	1.142
Mean		0.552	0.797	1.082	1.254	1.187	1.099
SD		0.0190	0.0228	0.0158	0.0386	0.0515	0.0232

Cables of the probes change*

*Twist the cables of the probes to check whether the signal cables of the probes have an influence on the measurement results.

Difference between calculation and measurements						
Setup	R1 [%]	R2 [%]	R3 [%]	R4 [%]	R5 [%]	B [%]
Planning [Gy]	0.533	0.766	1.084	1.239	1.081	1.158
MS 1	4.4	8.2	8.1	8.2	13.6	-1.2
MS 2	6.0	10.2	7.6	8.7	15.6	-2.9
MS 3	10.1	9.4	2.1	6.6	15.4	-4.6
MS 4	3.5	4.0	-0.2	1.2	9.9	-5.1
Mean	6.0	8.0	4.4	6.2	13.6	-3.5
SD	2.5	2.4	3.5	3.0	2.3	1.5

B Needle phantom Data

Table 21: Overview about the different project procedure for the needle phantom. The values in the table stand for the measurement days, the year was omitted.

Treatment	CC04	CC13	CC25	RAZOR Chamber	RAZOR Nano	RAZOR Diode	micro-Diamond	0.3 cm ³ Semiflex
max. Signal	20.01.	21.01.	29.01.	17.02.	11.02.	19.02.	24.02.	23.02. 24.02
Dose linearity of point-source	10.02.	29.01.	29.01.	17.02.	11.02.	19.02.	24.02.	23.02.
Different active lengths	12.02.	17.02.	12.02.	19.02.	12.02.	19.02.	24.02.	23.02.
Comparative measurements	10.03. 09.04.	10.03. 09.04.	10.03. 09.04.	09.04.	10.03. 09.04.	09.04.	10.03. 09.04.	10.03. 09.04.
Comparative of 2 and 4 needle	29.04.	30.04.	30.04.					
Number of measurements(n)	295	218	252	117	114	72	158	141

Results of the comparative measurements in the needle phantom

Treatment plan		Ion chamber	
OMP Plan	see Table	Manufacturer	-
TCC Plan	NORM_4Nadeln HDR	Model	see Table
Phantom	Needle	SN	-
Source calibration data			
Date	07.01.2021	Electrometer	
Activity [Ci]	11.10	iba	PTW UNIDOS (A)
SN	NLF01D85E5930	Dose ²	100298
		SN	10273

OMP = Oncentra Masterplan
N = Needle number

Chamber	Length [mm]	Time per position [s]	N1 [Gy]	N2 [Gy]	N3 [Gy]	N4 [Gy]	N4 correction with p_{TP} [Gy]	Mean [Gy]	Planning [Gy]	Deviation [%]
iba CC04	1110	130	0.636	1.224	1.831	2.422	2.460	2.459	2.456	0.11
SN 16286 (andere Kammer)			0.636	1.224	1.829	2.419	2.457			
iba CC13	1111	130	0.573	1.147	1.782	2.456	2.495	2.496	2.456	1.62
SN 16296			0.573	1.147	1.783	2.458	2.497			
iba CC25	1113	130	0.563	1.128	1.757	2.427	2.466	2.466	2.456	0.38
SN 16125			0.562	1.128	1.758	2.427	2.466			
iba RAZOR ^{Chamber}	1112	130	0.484	1.010	1.581	2.252	2.288	2.289	2.456	-6.79
SN 16294			0.485	1.101	1.584	2.255	2.291			
iba RAZOR ^{Nano Chamber}	1113	130	0.403	0.802	1.270	1.829	1.858	2.068	2.456	-15.81
SN 16233			0.488	0.967	1.493	2.047	2.079			
			0.486	0.958	1.480	2.024	2.056			
iba RAZOR ^{Diode Detector}	1104	130	0.5959	1.1724	1.7954	2.4298	2.4684	2.473	2.456	0.71
SN 10581			0.597	1.174	1.797	2.440	2.479			
PTW microDiamond			2.975E-09	5.853E-09	8.963E-09	1.213E-08	1.232E-08		[C]	
SN 123497 (UNIDOS (A))			2.979E-09	5.860E-09	8.969E-09	1.218E-08	1.237E-08			
PTW microDiamond	1104	130	0.640	1.232	1.833	2.421	2.459	2.458	2.456	0.09
SN 123497 (Dose ²)			0.641	1.231	1.831	2.419	2.457			
PTW 0.3 cm ³ Semiflex Chamber	1107	130	0.635	1.199	1.840	2.448	2.487	2.485	2.456	1.19
SN 0190 (UNIDOS (A))			0.545	1.099	1.700	2.349	2.424	2.424	2.456	-1.31
			0.544	1.092	1.700	2.348	2.423			

Date	09.04.2021
Source activity [Ci]	4.68
Total treatment time [s]	9880
Method	Timed continuous
Range	iba Low PTW High
Length [mm]	see Table
Air pressure [hPa]	1003.3
Temperature [°C]	21.8
P_{TP}	1.02
For 0.3 cm ³ Semiflex Chamber	
$N_{b,w}$	1.016

All CC's [Gy]	RAZOR Diode Detector [C]	Calibration factor [Gy/C]
2.473	1.235E-08	2.0032E+08
2.456		
0.71%		

C Water phantom Data

Table 22: Overview of the project procedure for the water phantom. The values in the table stand for the measurement days, the year was omitted.

Treatment	CC04	CC13	CC25	RAZOR Chamber	RAZOR Nano	RAZOR Diode	micro-Diamond	0.3 cm ³ Semiflex
max. Signal	14.04. 22.04.	07.04. 25.04. 26.04.	08.04. 14.04. 22.04. 23.04.	21.04.	15.04.	29.04.	25.02. 12.03. 16.03. - 18.03. 25.03.	08.04.
Dose linearity of point-source	14.04.	26.03.	08.04.	21.04.	15.04.		25.02.	
Point-source - depth dose	14.04.	25.03.	08.04.	21.04.	16.04.		11.03. 16.03. 17.03.	
Point-source - cross profile		26.03.	08.04.				11.03. 12.03.	
3 cm active length - depth dose	15.04.	26.03.	08.04.	21.04.	16.04.		12.03. 16.03.	
3 cm active length - cross profile		26.03.					12.03. 18.03	
5 cm active length - depth dose	15.04.	26.03. 16.04.	08.04. 22.04. 23.04.	21.04.	15.04.	29.04.	12.03.	
5 cm active length - cross profile	22.04.	26.03.	22.04.				18.03.	
8 cm active length - depth dose	14.04.	26.03.	14.04.	21.04.	16.04.		16.03. 17.03.	
8 cm active length - cross profile		26.03.					17.03.	
12 cm active length - depth dose	14.04.	07.04.	14.04.	21.04.	16.04.		17.03.	
12 cm active length - cross profile		07.04.					18.03.	
5 needles in triangular configuration	15.04. 28.04.	07.04.	14.03. 23.04.	21.04.	16.04.		25.03.	
Dependance on water heights		16.04.			16.04.			
Number of measurements(n)	155	304	203	96	109	73	642	59

5	10	15	20	25	30	35	40	45	50	55	60	65	70	75	80	85	90	95	100	105	110	115	120	125	130	135	140	145	150	155	160	165	170	175	180																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																																												
OMP_1Nadel-12cm	5.876	5.974	6.097	6.250	6.413	6.584	6.769	6.959	7.159	7.369	7.589	7.819	8.059	8.309	8.569	8.839	9.119	9.409	9.709	10.019	10.339	10.669	11.019	11.379	11.749	12.129	12.519	12.919	13.329	13.749	14.179	14.619	15.069	15.529	15.999	16.479	16.969	17.469	17.979	18.499	19.029	19.569	20.119	20.679	21.249	21.829	22.419	23.019	23.629	24.249	24.879	25.519	26.169	26.829	27.499	28.179	28.869	29.569	30.279	30.999	31.729	32.469	33.219	33.979	34.749	35.529	36.319	37.119	37.929	38.749	39.579	40.419	41.269	42.129	42.999	43.879	44.769	45.669	46.579	47.499	48.429	49.369	50.319	51.279	52.249	53.229	54.219	55.219	56.229	57.249	58.279	59.319	60.369	61.429	62.499	63.579	64.669	65.769	66.879	67.999	69.129	70.269	71.419	72.579	73.749	74.929	76.119	77.319	78.529	79.749	80.979	82.219	83.469	84.729	85.999	87.279	88.569	89.869	91.179	92.499	93.829	95.169	96.519	97.879	99.249	100.629	102.019	103.419	104.829	106.249	107.679	109.119	110.569	112.029	113.499	114.979	116.469	117.969	119.479	120.999	122.529	124.069	125.619	127.179	128.749	130.329	131.919	133.519	135.129	136.749	138.379	140.019	141.669	143.329	144.999	146.679	148.369	150.069	151.779	153.499	155.229	156.969	158.719	160.479	162.249	164.029	165.809	167.599	169.399	171.209	173.029	174.849	176.679	178.519	180.369	182.229	184.099	185.979	187.869	189.769	191.679	193.599	195.529	197.459	199.399	201.349	203.299	205.259	207.219	209.189	211.159	213.129	215.099	217.069	219.039	221.009	222.979	224.949	226.919	228.889	230.859	232.829	234.799	236.769	238.739	240.709	242.679	244.649	246.619	248.589	250.559	252.529	254.499	256.469	258.439	260.409	262.379	264.349	266.319	268.289	270.259	272.229	274.199	276.169	278.139	280.109	282.079	284.049	286.019	287.989	289.959	291.929	293.899	295.869	297.839	299.809	301.779	303.749	305.719	307.689	309.659	311.629	313.599	315.569	317.539	319.509	321.479	323.449	325.419	327.389	329.359	331.329	333.299	335.269	337.239	339.209	341.179	343.149	345.119	347.089	349.059	351.029	352.999	354.969	356.939	358.909	360.879	362.849	364.819	366.789	368.759	370.729	372.699	374.669	376.639	378.609	380.579	382.549	384.519	386.489	388.459	390.429	392.399	394.369	396.339	398.309	400.279	402.249	404.219	406.189	408.159	410.129	412.099	414.069	416.039	418.009	420.000	421.979	423.949	425.919	427.889	429.859	431.829	433.799	435.769	437.739	439.709	441.679	443.649	445.619	447.589	449.559	451.529	453.499	455.469	457.439	459.409	461.379	463.349	465.319	467.289	469.259	471.229	473.199	475.169	477.139	479.109	481.079	483.049	485.019	486.989	488.959	490.929	492.899	494.869	496.839	498.809	500.779	502.749	504.719	506.689	508.659	510.629	512.599	514.569	516.539	518.509	520.479	522.449	524.419	526.389	528.359	530.329	532.299	534.269	536.239	538.209	540.179	542.149	544.119	546.089	548.059	550.029	551.999	553.969	555.939	557.909	559.879	561.849	563.819	565.789	567.759	569.729	571.699	573.669	575.639	577.609	579.579	581.549	583.519	585.489	587.459	589.429	591.399	593.369	595.339	597.309	599.279	601.249	603.219	605.189	607.159	609.129	611.099	613.069	615.039	617.009	618.979	620.949	622.919	624.889	626.859	628.829	630.799	632.769	634.739	636.709	638.679	640.649	642.619	644.589	646.559	648.529	650.499	652.469	654.439	656.409	658.379	660.349	662.319	664.289	666.259	668.229	670.199	672.169	674.139	676.109	678.079	680.049	682.019	683.989	685.959	687.929	689.899	691.869	693.839	695.809	697.779	699.749	701.719	703.689	705.659	707.629	709.599	711.569	713.539	715.509	717.479	719.449	721.419	723.389	725.359	727.329	729.299	731.269	733.239	735.209	737.179	739.149	741.119	743.089	745.059	747.029	748.999	750.969	752.939	754.909	756.879	758.849	760.819	762.789	764.759	766.729	768.699	770.669	772.639	774.609	776.579	778.549	780.519	782.489	784.459	786.429	788.399	790.369	792.339	794.309	796.279	798.249	800.219	802.189	804.159	806.129	808.099	810.069	812.039	814.009	815.979	817.949	819.919	821.889	823.859	825.829	827.799	829.769	831.739	833.709	835.679	837.649	839.619	841.589	843.559	845.529	847.499	849.469	851.439	853.409	855.379	857.349	859.319	861.289	863.259	865.229	867.199	869.169	871.139	873.109	875.079	877.049	879.019	880.989	882.959	884.929	886.899	888.869	890.839	892.809	894.779	896.749	898.719	900.689	902.659	904.629	906.599	908.569	910.539	912.509	914.479	916.449	918.419	920.389	922.359	924.329	926.299	928.269	930.239	932.209	934.179	936.149	938.119	940.089	942.059	944.029	945.999	947.969	949.939	951.909	953.879	955.849	957.819	959.789	961.759	963.729	965.699	967.669	969.639	971.609	973.579	975.549	977.519	979.489	981.459	983.429	985.399	987.369	989.339	991.309	993.279	995.249	997.219	999.189	1001.159	1003.129	1005.099	1007.069	1009.039	1011.009	1012.979	1014.949	1016.919	1018.889	1020.859	1022.829	1024.799	1026.769	1028.739	1030.709	1032.679	1034.649	1036.619	1038.589	1040.559	1042.529	1044.499	1046.469	1048.439	1050.409	1052.379	1054.349	1056.319	1058.289	1060.259	1062.229	1064.199	1066.169	1068.139	1070.109	1072.079	1074.049	1076.019	1077.989	1079.959	1081.929	1083.899	1085.869	1087.839	1089.809	1091.779	1093.749	1095.719	1097.689	1099.659	1101.629	1103.599	1105.569	1107.539	1109.509	1111.479	1113.449	1115.419	1117.389	1119.359	1121.329	1123.299	1125.269	1127.239	1129.209	1131.179	1133.149	1135.119	1137.089	1139.059	1141.029	1142.999	1144.969	1146.939	1148.909	1150.879	1152.849	1154.819	1156.789	1158.759	1160.729	1162.699	1164.669	1166.639	1168.609	1170.579	1172.549	1174.519	1176.489	1178.459	1180.429	1182.399	1184.369	1186.339	1188.309	1190.279	1192.249	1194.219	1196.189	1198.159	1200.129	1202.099	1204.069	1206.039	1208.009	1210.000	1211.979	1213.949	1215.919	1217.889	1219.859	1221.829	1223.799	1225.769	1227.739	1229.709	1231.679	1233.649	1235.619	1237.589	1239.559	1241.529	1243.499	1245.469	1247.439	1249.409	1251.379	1253.349	1255.319	1257.289	1259.259	1261.229	1263.199	1265.169	1267.139	1269.109	1271.079	1273.049	1275.019	1276.989	1278.959	1280.929	1282.899	1284.869	1286.839	1288.809	1290.779	1292.749	1294.719	1296.689	1298.659	1300.629	1302.599	1304.569	1306.539	1308.509	1310.479	1312.449	1314.419	1316.389	1318.359	1320.329	1322.299	1324.269	1326.239	1328.209	1330.179	1332.149	1334.119	1336.089	1338.059	1340.029	1341.999	1343.969	1345.939	1347.909	1349.879	1351.849	1353.819	1355.789	1357.759	1359.729	1361.699	1363.669	1365.639	1367.609	1369.579	1371.549	1373.519	1375.489	1377.459	1379.429	1381.399	1383.369	1385.339	1387.309	1389.279	1391.249	1393.219	1395.189	1397.159	1399.129	1401.099	1403.069	1405.039	1407.009	1408.979	1410.949	1412.919	1414.889	1416.859	1418.829	1420.799	1422.769	1424.739	1426.709	1428.679	1430.649	1432.619	1434.589	1436.559	1438.529	1440.499	1442.469	1444.439	1446.409	1448.379	1450.349	1452.319	1454.289	1456.259	1458.229	1460.199	1462.169	1464.139	1466.109	1468.079	1470.049	1472.019	1473.989	1475.959	1477.929	1479.899	1481.869	1483.839	1485.809	1487.779	1489.749	1491.719	1493.689	1495.659	1497.629	1499.599	1501.569	1503.539	1505.509	1507.479	1509.449	1511.419	1513.389	1515.359	1517.329	1519.299	1521.269	1523.239	1525.209	1527.179	1529.149	1531.119	1533.089	1535.059	1537.029	1538.999	1540.969	1542.939	1544.909	1546.879	1548.849	1550.819	1552.789	1554.759	1556.729	1558.699	1560.669	1562.639	1564.609	1566.579	1568.549	1570.519	1572.489	1574.459	1576.429	1578.399	1580.369	1582.339	1584.309	1586.279	1588.249	1590.219	1592.189	1594.159	1596.129	1598.099	1600.069	1602.039	1604.009	1605.979	1607.949	1609.919	1611.889	1613.859	1615.829	1617.799	1619.769	1621.739	1623.709	1625.679	1627.649	16

